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The effect eccentric phase duration on maximal strength, muscular hypertrophy and countermovement jump: A systematic review and meta-analysis

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1

8 ABSTRACT

9 Some authors suggest slower eccentric tempos enhance resistance training (RT) adaptations, and

- 10 narrative reviews yield divergent conclusions. PubMed, CINAHL, SPORTDiscus, ProQuest, and
- 11 Google Scholar were searched following Cochrane Handbook and PRISMA-guidelines, to compare
- 12 RT outcomes following fast (FEG) and slow (SEG) eccentric phases. Random-effects multi-level
- 13 meta-analyses with robust variance estimation was performed for strength, hypertrophy, and
- 14 countermovement jump (CMJ), with results interpreted relative to a region of practical
- 15 equivalence. Evidence quality was assessed using the Cochrane RoB 2 and GRADE criteria. Eight
- 16 studies involving 148 participants (52% trained, 80% male) were included. FEG enhanced CMJ by a
- 17 practically worthwhile degree with moderate certainty (Hedge's g = -0.73 [90% Cl = -1.34, -0.12;
- 18 90% PI = -1.34, -0.12]), while uncertain estimates for maximal strength (g = 0.18 [90% CI = -0.27,
- 19 0.63; 90% PI = -0.96, 1.31]) and muscle hypertrophy (g = 0.03 [90% CI = -0.30, 0.36; 90% PI = -0.32,
- 20 0.38]) meant that practically worthwhile effects could neither be supported nor rejected. SEG led
- 21 to practically equivalent or enhanced strength gains, compared to FEG, in trained participants (g =
- 22 0.33 [90% CI = 0.07, 0.60; 90% PI = 0.07, 0.60]) and volume-load matched trials (g = 0.25 [90% CI =
- 23 0.04, 0.45; 90% PI = 0.04, 0.45]) with moderate certainty in subgroup analyses. FEG may enhance
- CMJ, while SEG may cause similar or higher maximal strength increases in trained participants
- and volume-load matched conditions. Given the uncertainty of estimates, more research is
- 26 needed. This project was prospectively registered (<u>https://osf.io/s6uqn/</u>).





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27 **1. INTRODUCTION**

Resistance training (RT) is the best-known tool to induce robust strength and hypertrophy
adaptations. These adaptations are influenced by numerous variables, including volume [1], load
[2], and proximity-to-failure [3], among others. However, the impact of tempo (i.e., total and
phase-specific repetition speed) has received relatively little attention.

32

Schoenfeld and colleagues reported extremely slow repetitions (>10 seconds per repetition)
produced inferior muscle hypertrophy compared to faster durations (0.5-8 seconds) [4].
Subsequent reviews reported mixed strength and hypertrophy results comparing fast and
moderately slow execution tempos [5,6]. Notably, these conclusions were based on a limited
number of studies, and many combined forms of tempo manipulation. Thus, it remains
challenging to determine distinct effects of altering specific repetition-phase duration versus
overall repetition duration.

40

Emerging evidence suggests individual contraction phase speed may be more relevant for strength and hypertrophy. For instance, a recent meta-analysis found greater strength gains when concentric phases were performed rapidly (<2 seconds) compared to slower (\geq 2 seconds) (ES = 0.21, p = 0.029) [7]. Therefore, faster concentric contractions may better enhance strength, potentially because efforts to slow concentric duration increases difficulty, diminishes neuromuscular performance, and possibly lowers motor unit recruitment, irrespective of total

- 47 repetition duration [8–10].
- 48

49 Conversely, the impact of extending eccentric phases is less studied. Eccentric-only actions can 50 produce greater or similar magnitudes of hypertrophy than concentric-only contractions and combined eccentric-concentric actions, respectively [11,12]. While slowing the eccentric phase 51 52 can reduce RT performance [13–16], this acute performance decline may not negatively impact 53 long-term adaptations [17]. Considering eccentric actions require less energy and eccentric 54 strength is higher than concentric [18], but this strength differential decreases as eccentric 55 duration increases [19], greater time under tension or impulse (force \times time) per set could potentially be achieved by slowing eccentric duration to a point, making the "cost" of doing so 56 possibly worthwhile. Consequently, slowing the eccentric – to a degree - while maintaining faster 57 58 concentric contractions may promote greater hypertrophy without impeding strength 59 improvements. 60





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To date, two reviews have qualitatively addressed the impact of slowing down the eccentric
duration [10,20], yielding differing conclusions. In addition, study quality assessments were not
performed. Given the inconsistency and gaps in the literature, a meta-analytic approach may be

64 more appropriate to assess the impact of different eccentric tempos on muscular performance

65 and hypertrophy. Thus, we conducted a systematic review with meta-analysis seeking to

66 quantitatively evaluate the impact of varying eccentric tempos on indices of muscular

- 67 performance and hypertrophy.
- 68

69 **2. METHOD**

70 **2.1 Overview and registration**

71 This systematic review was performed in accordance with the *Cochrane Handbook for Systematic*

72 *Reviews of Interventions* (version 6.4.0) and the Preferred Reporting Items for Systematic Reviews

and Meta-Analyses (PRISMA) statement [21] guidelines. The review was prospectively registered

on the Open Science Framework after pilot searches (<u>https://osf.io/s6uqn/</u>), but before any formal

75 searches or record screening.

76 2.2 Search strategy

77 A comprehensive search strategy using various terms related to resistance exercise and eccentric 78 phase duration was developed in accordance with the PRISMA-S checklist [22], assisted by three 79 specialised tools: the Word Frequency Analyzer (<u>https://sr-accelerator.com/#/wordfreg</u>), Research 80 Refiner (https://sr-accelerator.com/#/searchrefinery), and Polyglot Search Translator (https://sr-81 accelerator.com/#/polyglot) [23,24]. The searches were conducted from inception to November 10th, 2023 in PubMed/MEDLINE, SCOPUS, SPORTDiscus, CINAHL, ProQuest, and Google Scholar. 82 83 Search results from Google Scholar was mass exported using the Publish or Perish software [25]. This comprehensive approach was designed to maximise the chances of locating both peer-84 85 reviewed and grey literature. For Google Scholar, the search was limited to the first 1,000 hits 86 (980 results were retrieved due to software error), and for ProQuest, searches were limited to 87 scholarly journals, dissertations, and theses. No other predefined limits or filters were applied. 88 The full search strings can be found in **Supplementary file 1**. Additionally, secondary searches 89 were performed, including: 1) Screening reference lists of all included studies and relevant review 90 papers; 2) Forward citation tracking through Google Scholar for the included studies; and 3) 91 Ongoing search alerts after the initial search date until the week before submission.





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92 **2.3 Text screening and selection**

After removal of duplicates, titles and abstracts were independently screened for eligibility by the 93 94 two researchers (CA and AK) using the systematic review software Rayyan (https://rayyan.ai/). 95 Disagreements were resolved through discussion. For all remaining articles, full-texts were 96 included if they investigated the impact of eccentric phase duration as the independent variable, classified as either fast (i.e., ≤2 sec or maximal intent) or slow (i.e., >2 sec), and 1) were published 97 98 in a peer-reviewed journal, on a pre-print repository, or as a Master's or PhD thesis; 2) written in 99 English; 3) included healthy human participants with no disease or musculoskeletal injury; 4) used 100 parallel groups or contralateral, within-participants designs to assess the effects of altered eccentric phase duration on indices of muscle strength, power, endurance, and/or hypertrophy; 101 5) used traditional combined eccentric/concentric isotonic contractions; 6) matched the duration 102 103 of all contraction phases except the eccentric (i.e. concentric and possible isometric transition 104 phases); 7) attempted to match frequency, relative-load (% of 1RM or RM relative to tempo), and 105 volume (number of sets or volume-load) between groups; and 8) were at least 4 weeks long. 106 Studies employing eccentric-only and overloaded eccentrics were excluded.

107 **2.4 Study coding and extraction**

108 The following data were extracted from the included studies: 1) number of participants and their age, sex, and training experience; 2) RT protocol including duration, frequency, volume, relative-109 110 load, rest periods, and exercise selection; 3) study design; 4) tempo of each contraction phase; 5) outcome measures; 6) the presence of concurrent training; and 7) mean changes and standard 111 112 deviations of the relevant indices of muscular performance and hypertrophy, as well as withingroup correlations of pre-post scores. Where insufficient data were reported, corresponding 113 114 authors were contacted by email twice over two months. If they failed to provide the required 115 data, data were extracted using WebPlotDigitizer and/or calculated in accordance with the 116 Cochrane Handbook [26]. All data extraction was completed by CA and coding files were cross-117 checked by AK for accuracy and differences were resolved through discussion and consensus.

118 **2.5 Risk of bias assessment**

119 Risk of bias (RoB) was performed using the second version of the Cochrane RoB tool for

- 120 randomised trials (RoB 2) [27], in accordance with the Cochrane Handbook [28]. The effect of
- 121 adhering, not assignment, to the protocol was the effect of interest. Studies were categorised as:
- 122 "Low risk of bias" if all domains were assessed as low risk; "Some concerns" if concerns were
- 123 raised in one domain, but no domain was determined to be high risk; "High risk of bias" if at least





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124 one domain was classified as high risk or if multiple domains raised some concern. The Grading of Recommendations Assessment, Development and Evaluation (GRADE) system was used to 125 evaluate evidence certainty for studies included in the quantitative synthesis, using the GRADEpro 126 127 GDT software [29], in accordance with the GRADE [30] and Cochrane [31] handbooks, including guidance updates for inconsistency [32] and imprecision [33]. Both RoB and GRADE assessment 128 129 was performed independently by two researchers (CA and AK). Disagreements were resolved 130 through discussion.

131

132 2.6 Statistical analysis

133 2.6.1 Multi-level synthesis

Quantitative synthesis was performed for separate outcomes when reported by at least two 134 135 studies. Analyses were performed using R Statistical Software (v4.3.0; R Core Team 2021) [34]. Given that multiple effect sizes were reported in included studies (e.g., more than one slower 136 137 eccentric phase duration or multiple measures for the same outcome within a study), a threelevel (i.e., study, group, and outcome) mixed-effect meta-analysis with robust variance estimation 138 139 were fitted with *metafor* [35] and *clubSandwich* [36] packages. All multi-level meta-analysis models 140 were based on a t-distribution due to the small sample sizes of the included studies [37]. Model parameters were estimated using restricted maximum likelihood estimation. Effect sizes were 141 142 weighted based on their inverse sampling variance. A within-study effect size sampling error correlation coefficient of $\rho = 0.6$ was assumed for robust variance estimation. Sensitivity analyses 143 with lower ($\rho = 0.4$) and higher ($\rho = 0.8$) values were performed to check robustness. Sufficient 144 145 studies were found for maximal strength, hypertrophy, and countermovement jump height (CMJ). For all multi-level models, l^2 and τ^2 were calculated to guantify relative and absolute between 146 study heterogeneity, respectively. l^2 and τ^2 were partitioned across levels 2 (within-study) and 3 147 148 (between study) of the multi-level meta-analysis. Publication bias was assessed using the multi-149 level extension of the Egger's test [38] and by funnel plot visual inspection for observed effect 150 sizes and conditional residuals [39].

151

152 Pre-planned subgroup analyses were performed for i) study design (categorical: between- and

153 within-participant designs) and ii) training status (categorical: trained and untrained), while

154 exploratory subgroup and moderator analyses were performed when at least two studies were

- 155 represented in each subgroup, based on visual inspection of the forest plot and the study
- 156 characteristics. These subgroups were: i) exercise selection (categorical: multi-joint and single-





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157 joint), ii) muscle group (categorical: elbow flexor and anterior thigh), iii) volume matching

158 (categorical: sets to failure and volume-load).

159 **2.6.2 Effect size calculation**

- Due to the different tests used to measure maximal strength (e.g., Scott curl, back squat, etc.), 160 161 hypertrophy (e.g., ultrasound and MRI), and CMJ (e.g., with or without arm swing), calculating a standardised mean difference (SMD) was deemed more appropriate than using raw mean 162 differences. SMD with a small sample size correction (Hedges' g) was calculated, in accordance 163 164 with Borenstein and colleagues [40], such that a positive effect size favoured SEG. To account for the inter-dependencies of effects in within-participant designs, separate effect size calculations 165 166 were used for between-participant (i.e., parallel group designs [equations 1-3]) and withinparticipant designs (i.e., contralateral limb designs [equations 4-7]), and then combined in the 167
- 168 final analysis [40].

Equation 3:

169 Equation 1:

171

176

$$g = \frac{\overline{x_1} - \overline{x_2}}{SD_{pooled}} J,$$

$$SD_{pooled} = \sqrt{\frac{(n_1 - 1)SD_1^2 + (n_2 - 1)SD_2^2}{n_1 + n_2 - 2}},$$

$$J = 1 - \frac{3}{4(n_1 + n_2 - 2) - 1'}$$

where $\overline{X_1}$ and $\overline{X_2}$ are the mean group change scores, SD_{pooled} is the pooled standard deviation, *J* is a small sample size correction, and n_1 and n_2 are the sample sizes of each group.

- 174 Equation 4: $g = \frac{\overline{Y_1} \overline{Y_2}}{SD_{nooled}} J,$
- 175 Equation 5: SD

$$SD_{pooled} = \frac{S_{diff}}{\sqrt{2(1-r)'}}$$
$$SD_{diff} = \sqrt{SD_1^2 + SD_2^2 - 2 * r * SD_1 * SD_2},$$

177 Equation 7:

Equation 6:

 $SD_{diff} = \sqrt{SD_1^2 + SD_2^2 - 2 * r * SI}$ $J = 1 - \frac{3}{4(n-1)-1'}$

where $\overline{Y_1}$ and $\overline{Y_2}$ are the mean change scores for each limb, SD_{diff} is the standard deviation of the within-participant difference between change scores, and *r* is correlation of the between-limb

180 within-participant change scores.

181 **2.6.3 Model Diagnostics**

- 182 To identify potential outliers and influential observations, Cook's distance and hat values were
- 183 calculated in *metafor* [35]. Model diagnostics were not performed for jump height due to the
- small number of included studies (k = 3). Cook's distance was judged according to the F
- 185 distribution where $\alpha = 0.50$ and [41]:





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- df = (k+1, n k 1)186 187 Hat values (*h*) were deemed noteworthy where exceeding twice the average [42]: $\overline{h} = \frac{k+1}{n}$ 188 189 Where potential outliers or influential observations were identified, a separate meta-analysis was performed with the corresponding potential outlier/influential study removed and the results 190 191 were compared to the main meta-analysis to check the interpretation (i.e., direction of effect, 192 confidence [CI] and prediction intervals [PI]) [43]. This check was conducted as a sensitivity 193 analysis since it is not possible to distinguish between (large) sampling error and true outliers
- 194 [44].

195 **2.6.4 Statistical inferences**

- A limitation of traditional meta-analyses with null hypothesis significance testing (NHST) is that 196 they can reject the absence of an effect but cannot support it [45,46]. This often leads to 197 erroneous conclusions of 'no effect' when no statistically significant differences are observed. A 198 199 non-significant difference may simply indicate substantial uncertainty and the need for additional 200 research [46,47]. Therefore, we adopted equivalence and minimum effects procedures [45,48], 201 within an estimation-based approach [49]. As such, the practical implications of all results compatible with the data, including their precision (90% CI and PI), were interpreted, relative to 202 203 our region of practical equivalence (ROPE) [48]. Evidence of no practically worthwhile effects is supported if the point estimate and its entire 90% CI and PI falls within our ROPE (i.e., effects are 204 205 practically equivalent to zero) [45]. Conversely, to support a practically worthwhile effect, the point estimate and its entire 90% CI and PI must fall outside of our ROPE. Any 90% CIs and PIs that 206 overlap with our ROPE are considered uncertain, making the absence or presence of practically 207 208 worthwhile effects unclear. Inferences from equivalence and minimum effects procedures are normally only interpreted relative to the 90% CI [48]. To account for between-study 209 210 heterogeneity, 90% PIs were also used to understand the precision and reliability of the point 211 estimate from included studies (CI), as well as the possible range of effects when applying the 212 results of this meta-analysis to new studies or practical scenarios (PI). However, 95% CI, 95% PI and *p*-values (two-tailed NHST) were reported to allow readers to interpret results through their 213 214 preferred lens, but they did not influence our inferences, except for GRADE imprecision [33]. 215 We based our ROPEs on meta-analytic data [1,50], with effects less than ±0.25, ±0.28, and ±0.11 216
- 217 for maximal strength, hypertrophy, and CMJ, respectively, considered practically not worthwhile.
- These thresholds align with the 25th percentile of RT effects on the given outcomes [50]. Although





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no specific recommendations were provided for hypertrophy, the 95% credible interval (0.10 to 0.66) of RT vs. control for hypertrophy from 119 studies by Currier and colleagues [1] was used to estimate the 25th percentile of effects, assuming a normal distribution. The same data were also used to delineate small (maximal strength: 0.25 to <0.59; hypertrophy: 0.28 to <0.38; CMJ: 0.11 to <0.38), moderate (50th percentile [maximal strength: 0.59 to <0.98; hypertrophy: 0.38 to <0.48; CMJ: 0.38 to <0.67]), and large (75th percentile [maximal strength: \ge 0.98; hypertrophy: \ge 0.48; CMJ: \ge 0.67]) effect size magnitudes for each outcome.

227 **3. Results**

228 **3.1 Selection of sources of evidence**

Our systematic search yielded 3227 results. After removing duplicates, 2195 articles were eligible 229 230 for title and abstract screening. Subsequently, 48 articles underwent full-text review, with 38 231 excluded due to: i) non-accessible full-text, ii) incorrect study design, iii) combined ECC-CON 232 isotonic contractions not performed, iv) no manipulation of eccentric tempo, v) lack of matched 233 concentric tempo between groups, and vi) comparison of two eccentric tempos, both of which 234 considered slow by the inclusion criteria. Consequently, 9 articles were included, with two 235 reporting data from the same study, resulting in 8 unique studies [17,51–57]. For PRISMA-236 flowchart, see Figure 1. Additional data was requested from all first and/or corresponding 237 authors, of which all but one [52] responded. As such, mean changes, change SD, correlations of 238 within-group pre-post scores and within-participant between-limb change scores (for withinparticipant designs) or sufficient data to estimate them were provided either directly by authors 239 240 [51,53], calculated from raw data [17,54–57] or estimated from extracted full-text data [52], in accordance with the Cochrane Handbook [26]. 241





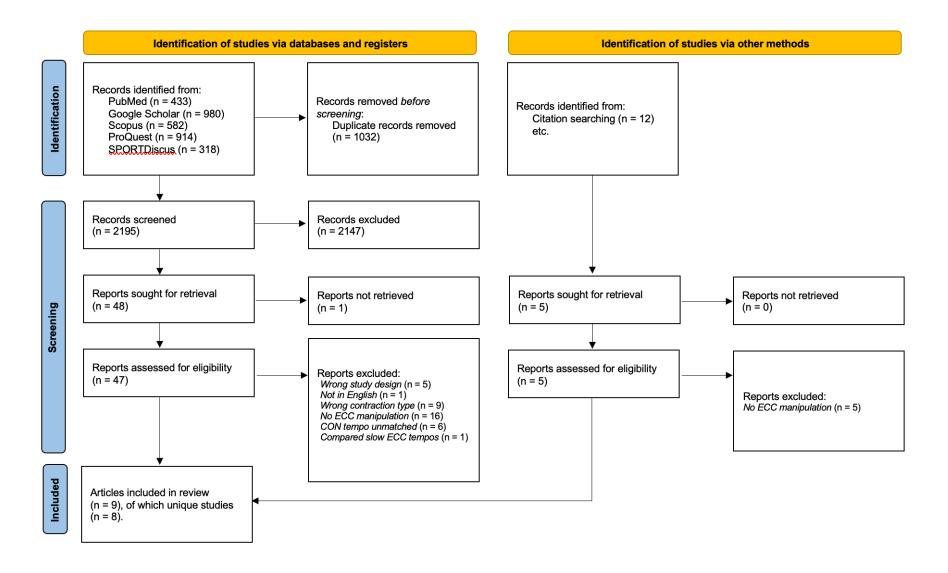


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244 **Fig. 1** PRISMA-flowchart. *ECC* eccentric tempo, *CON* control





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245 **3.2 Study characteristics**

The pooled number of participants across all studies was 148, of which 52% (n = 77) and 80% (n = 246 118) were resistance-trained and male, respectively. The median sample size per comparator 247 248 group was 10 participants (range: 6-13). Two studies employed a within-participants design 249 [56,57], while the remaining utilised a parallel-groups design. The median intervention period was 250 7.5 weeks (range: 4-12 weeks). All studies required participants to train twice weekly, with a 251 median 3.5 sets per exercise (range: 2-5 sets). Two studies incorporated 5-7 exercises per session 252 [51,54], while the rest included one. The fast eccentric groups (FEG) maintained a median tempo 253 of 1.25 seconds (range: 1-2 seconds) and 1 second (range: 1-2 seconds) in the eccentric and 254 concentric parts of the movement, respectively. The slow eccentric groups (SEG) took a median 4 255 seconds (range: 3-6 seconds) and 1 second (range: 1-2 seconds) to lower and lift the weight, 256 respectively. Four studies matched volume-load (sets × repetitions × load) between groups 257 [51,52,54,56], allowing for variations in proximity-to-failure. The remaining four had groups 258 perform an equal number of sets to failure [17,53,55,57], allowing differences in performed 259 repetitions or absolute load. All studies evaluated 1RM strength, on either the free-weight [53,54] or smith-machine [52] back squat, leg press [51], leg extension [51,56,57], or Scott curl [17,55]. 260 261 Five studies measured hypertrophy of the elbow flexors [17,55] or anterior thigh [53,56,57] using 262 ultrasound [17,55–57] or MRI [53]. Three studies assessed countermovement jump (CMJ) [52–54]. 263 Tensiomyography [55], squat jump [53], loaded CMJ [52], functional capacity tests (6 m walk, 264 timed up-and-go, stair-climbing, and stair-rising) [51], 20 m sprint [54], 505 agility [54], T-test [53], 265 and Yo-Yo intermittent recovery test level 2 [53] were also assessed. However, these results were 266 not extracted for meta-analysis due to an insufficient number of studies. An overview of the 267 studies is available in Table 1.





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268Table 1 Study overview

Study	Participants	Training protocol	Tempo (s) [ECC/ISO/CON]	Primary outcome(s)
Dias et al.,	FEG: 68 ± 7 y	Exercise/s:	FEG:	Strength: 1RM leg press and leg
2015	<i>n</i> = 10F	Leg press, leg extension, among others*.	1.5/0/1.5 SEG:	extension.
	SEG: 66 ± 6 y	Prescription:	4.5/0/1.5	
	n = 9F	12 weeks, 2 sessions/week.		
	RT experience: Untrained	2-3 sets of 8-12 repetitions at 45-70% of 1RM, 2-3 mins inter-set rest.		
Pereira et al.,	FEG: 28 ± 8 y	Exercise/s:	FEG:	Strength: 1RM Scott curl;
2016	n = 6M	Scott curl.	1/0/1 SEG:	Hypertrophy: Biceps brachii MT via US.
	SEG: 30 ± 6 y	Prescription:	4/0/1	
	n = 6M	12 weeks, 2 sessions/week.3 sets of 8 repetitions at 8RM, 2 mins inter-set rest.		
	RT experience: Trained (≥1 y)	5 Sets of 6 repetitions at orticity 2 minis inter set rest.		
Mike et al.,	FEG: 22 ± 2 y	Exercise/s:	FEG:	Strength: 1RM Smith machine squat;
2017	<i>n</i> = 10M	Smith machine squat.	2/1/2 SEG1:	Power: CMJ.
	SEG1: 22 ± 2 y	Prescription:	4/1/2	
	n = 9M	4 weeks, 2 sessions/week. 4 sets of 6 repetitions at 80-85% of 1RM, 3 mins	SEG2: 6/1/2	
	SEG2: 23 ± 4 y n = 11M	inter-set rest.	0/1/2	





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	RT experience: Trained (≥3 y)			
Kojić et al.,	FEG: 28 ± 8 y	Exercise/s:	FEG:	Strength: 1RM Scott curl;
2021	n = 6M, 4F	Scott curl.	1/0/1	Hypertrophy: Biceps brachii MT via US
			SEG:	
	SEG: 30 ± 6 y	Prescription:	4/0/1	
	<i>n</i> = 5M, 5F	7 weeks, 2 sessions/week.		
		3-4 sets at 60-70% of 1RM to failure, 2 mins inter-		
	RT experience:	set rest.		
	Untrained			
Shibata et al.,	FEG: 20 ± 1 y	Exercise/s:	FEG:	Strength: 1RM back squat;
2021	<i>n</i> = 11M	Back squat.	2/0/2	Hypertrophy: Quadriceps CSA at 30%,
		-	SEG:	50% and 70% of femur length via MRI;
	SEG: 20 ± 1 y	Prescription:	4/0/2	Power: CMJ.
	n = 11M	6 weeks, 2 sessions/week.		
		3 sets at 75% of 1RM to failure, 3 mins inter-set		
	RT experience:	rest.		
	Untrained			
Pearson et	FEG: 23 ± 10 y	Exercise/s:	FEG:	Strength: 1RM unilateral leg extension;
al., 2022	<i>n</i> = 13M	Unilateral leg extension.	1/0/1	Hypertrophy: Anterior thigh MT at 40%
		-	SEG:	and 60% of femur length via US.
	SEG: 23 ± 10 y	Prescription:	3/0/1	C
	<i>n</i> = 13M	8 weeks, 2 sessions/week.		
		3-4 sets of 8-10 repetitions at 8-10RM, 2 mins		
	RT experience:	inter-set rest.		
	Trained ($\geq 3 \text{ y}$)	Within-participants design.		





Azevedo et	FEG: 25 ± 5 y	Exercise/s:	FEG:	Strength: 1RM unilateral leg extension;
al., 2022	n = 8M, 2F	Unilateral leg extension.	2/0/1	Hypertrophy: Rectus femoris, vastus
	SEG: 25 ± 5 y n = 8M, 2F	Prescription: 8 weeks, 2 sessions/week.	SEG: 4/0/1	medialis and vastus lateralis MT via US.
	RT experience: Untrained	5 sets at 70% of 1RM to failure, 3 mins inter-set rest. Within-participants design.		
Segers et al.	FEG: 22 ± 3 y	Exercise/s:	FEG:	Strength: 1RM back squat;
2022	<i>n</i> = 11M	Back squat, hex bar deadlift, among others.	1/0/X SEG:	Power: CMJ.
	SEG: 22 ± 3 y	Prescription:	4/0/X	
	<i>n</i> = 11M	4 weeks, 2 sessions/week.	X = maximal	
	RT experience: Trained (≥2 y)	3-4 sets of 3-4 repetitions at 70-80% of 1RM.	intent	

269 * 'Among others' indicate that other exercises were also performed, typically as part of a whole-body routine, but were either irrelevant

for the measured outcomes or not subject to tempo manipulation. RT resistance training, ECC eccentric, ISO isometric, CON concentric,

271 *M* males, *F* female, *RM* repetition maximum, *CMJ* countermovement jump, *MT* muscle thickness, *US* ultrasound



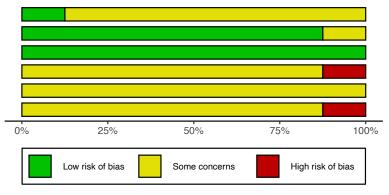


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272 **3.3 Study quality and certainty of evidence**

273 One study [56] had a low risk of bias regarding the randomisation process, while the remaining 274 seven studies were rated as "some concerns" due to insufficient information about randomisation 275 procedures and allocation sequence concealment. For deviations from intended interventions, 276 seven studies had a low risk of bias. One study [17] had some concerns due to a lack of blinding 277 and insufficient information about external training influences. All studies had a low risk of bias 278 concerning missing outcome data, as either no dropouts or equally distributed dropouts were reported. Regarding the measurement of outcomes, one study [17] had a high risk of bias for 279 280 strength measurements, while seven had some concerns. For hypertrophy outcomes, three 281 studies [17,55,57] had some concerns, while two had a low risk of bias [53,56]. Regarding power measurements, one study was low risk [53], while the remaining two had some concerns [52,54]. 282 283 The primary sources of bias in these domains were lack of blinding of assessors and use of 284 methods susceptible to human influence. All studies had some concerns related to the selection 285 of reported results because none had pre-registered methods, making it impossible to assess 286 deviations from a specified plan. In summary, one study [17] had a high overall risk of bias, while 287 the remaining seven studies had some concerns overall (Figure 2, Supplementary files 2 and 3). 288 Funnel plot visual inspection did not suggest publication bias (Supplementary file 3), which was 289 corroborated by the Egger's test for maximal strength (p = 0.75), hypertrophy (p = 0.31), and CMI 290 (p = 0.39). The certainty of evidence for pooled and subgroup analyses can found in Table 2 and 291 Supplementary file 4.

Bias arising from the randomization process Bias due to deviations from intended interventions Bias due to missing outcome data Bias in measurement of the outcome Bias in selection of the reported result Overall risk of bias



292293 Fig. 2 Risk of bias assessment





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294 **3.4 Quantitative analysis**

295 3.4.1 Maximal strength

- The pooled analysis for maximal strength revealed that the average effect most compatible with our data, given our statistical model, was a practically not worthwhile effect favouring SEG with poor precision (Figure 3). The effect size ranged from a small effect favouring FEG to a moderate
- effect favouring SEG (0.18 [90% CI = -0.27, 0.63; 90% PI = -0.96, 1.31; 95% CI = -0.39, 0.74; 95% PI
- 300 = -1.24, 1.60], p = 0.48, $l^2_{\text{within}} = 0\%$, $l^2_{\text{between}} = 65.8\%$, $\tau^2_{\text{within}} < 0.01$, $\tau^2_{\text{between}} = 0.30$). Considering our
- 301 ROPE (±0.25), the 90% CI, and 90% PI, these results are highly uncertain, and the presence or
- 302 absence of a practically worthwhile effect of eccentric tempo manipulation on maximal strength
- 303 can neither be supported nor rejected.
- 304 Subgroup analyses found small effects with poor precision, ranging from practically not
- 305 worthwhile to small or moderate effects favouring SEG. This was observed when i) participants
- 306 were trained (0.33 [90% CI = 0.07, 0.60; 90% PI = 0.07, 0.60]), and ii) volume-load was matched
- 307 (0.25 [90% CI = 0.05, 0.44; 90% PI = 0.05, 0.44]). Considering our ROPE (±0.25), the 90% CI, and
- 308 90% PI, SEG does not practically harm maximal strength gains in these subgroups, but whether it
- 309 enhances maximal strength gains by a practically worthwhile degree cannot be inferred with
- 310 certainty.
- 311 The remaining subgroup analyses and moderator analyses found practically not worthwhile to
- 312 small average effects, with very poor precision, ranging from small to large in both directions
- 313 (Tables 2 and 3). Considering our ROPE (±0.25), the 90% CI, and 90% PI, these results are highly
- 314 uncertain, and the presence or absence of a practically worthwhile effect of eccentric tempo
- 315 manipulation on maximal strength cannot be supported or rejected.



Estimate [90% CI]

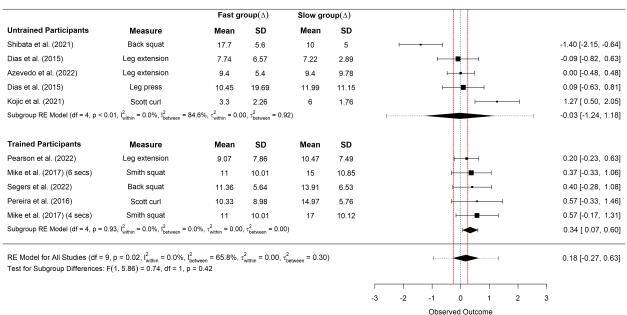


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316

- 317 Fig. 3 Forest plot for pooled maximal strength analysis, including subgroup and moderator
- analysis for training status. The red lines represent the lower and upper bounds of our region of
- 319 practical equivalence (±0.25). Cl confidence interval, SD standard deviation

320 3.4.2 Muscle hypertrophy

- 321 The pooled analysis for hypertrophy revealed that the average effect most compatible with our
- data, given our statistical model, was a practically not worthwhile effect favouring SEG with poor
- 323 precision (Figure 4). The effect size ranged from a moderate effect favouring FEG to a large effect
- 324 favouring SEG (0.03 [90% CI = -0.30, 0.36; 90% PI = -0.32, 0.38; 95% CI = -0.42, 0.48; 95% PI = -
- 325 0.45, 0.51], p = 0.86, $l^2_{\text{within}} = 0.0\%$, $l^2_{\text{between}} = 2.2\%$, $\tau^2_{\text{within}} < 0.01$, $\tau^2_{\text{between}} < 0.01$). Considering our
- ROPE (±0.28), the 90% CI, and 90% PI, these results are highly uncertain, and the presence or
- 327 absence of a practically worthwhile effect of eccentric tempo manipulation on hypertrophy can328 neither be supported nor rejected.
- 329 Subgroup analyses and moderator analyses found practically not worthwhile to moderate
- average effects with very poor precision and large effects in both directions (**Tables 2** and **3**).
- Considering our ROPE (±0.28), the 90% CI, and 90% PI, these results are highly uncertain, and the





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332 presence or absence of a practically worthwhile effect of eccentric tempo manipulation on

333 hypertrophy cannot be supported or rejected.

334

Azevedo et al. (2022) VL MT 4.28 2.81 3.53 2.86 -0.12 [-0.59, 0.36] Pearson et al. (2022) Anterior thigh MT (40%) 0.24 0.29 0.21 0.32 Azevedo et al. (2022) RF MT 2.02 2.1 2.84 2.37 Azevedo et al. (2022) VM MT 2.37 1.42 4.29 1.97 Subgroup RE Model (df = 4, p = 0.29; $l_{wtthin}^2 = 5.0\%$, $l_{between}^2 = 0.0\%$, $\tau_{wtthin}^2 = 0.00$, $\tau_{between}^2 = 0.00$) -0.54 [-1.23, 0.15] Between-participant Measure Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $l_{wtthin}^2 = 0.0\%, l_{between}^2 = 69.6\%, \tau_{wtthin}^2 = 0.00, \tau_{between}^2 = 0.45) 0.25 [-1.13, 1.62] $			Fast gr	oup(Δ)	Slow gr	oup(\Delta)							
Azverdo et al. (2022) VL MT 4.28 2.81 3.53 2.86 Pearson et al. (2022) Anterior thigh MT (40%) 0.24 0.29 0.21 0.32 Azverdo et al. (2022) RF MT 2.02 2.1 2.84 2.37 Azverdo et al. (2022) VM MT 2.37 1.42 4.29 1.97 Subgroup RE Model (df = 4, p = 0.29; $l_{wthin}^2 = 5.0\%$, $l_{between}^2 = 0.0\%$, $\tau_{between}^2 = 0.00$) Between-participant Measure Mean SD Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.29; $l_{wthin}^2 = 0.0\%$, $l_{between}^2 = 0.00$, $\tau_{between}^2 = 0.45$) RE Model for All Studies (df = 9, p = 0.29; $l_{wthin}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{wthin}^2 = 0.00$, $\tau_{between}^2 = 0.00$) RE Model for All Studies (df = 9, p = 0.29; $l_{wthin}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{wthin}^2 = 0.00$, $\tau_{between}^2 = 0.00$)	Within-participant	Measure	Mean	SD	Mean	SD							
Pearson et al. (2022) Anterior thigh MT (40%) 0.24 0.29 0.21 0.32 Azevedo et al. (2022) RF MT 2.02 2.1 2.84 2.37 Azevedo et al. (2022) VM MT 2.37 1.42 4.29 1.97 Subgroup RE Model (df = 4, p = 0.29; $l_{within}^2 = 5.0\%$, $l_{between}^2 = 0.0\%$, $r_{within}^2 = 0.00$, $r_{between}^2 = 0.00$) Between-participant Measure Mean SD Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 69.6\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.00$) RE Model for All Studies (df = 9, p = 0.29; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 0.2\%$, $\tau_{within}^2 = 0.0\%$, $\tau_{between}^2 = 0.00$) RE Model for All Studies (df = 9, p = 0.29; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 0.2\%$, $\tau_{within}^2 = 0.0\%$, $r_{between}^2 = 0.00$)	Pearson et al. (2022)	Anterior thigh MT (60%)	0.28	0.34	0.13	0.32		⊢	-∎				-0.21 [-0.63, 0.22]
Azevedo et al. (2022) RF MT 2.02 2.1 2.84 2.37 Azevedo et al. (2022) VM MT 2.37 1.42 4.29 1.97 Subgroup RE Model (df = 4, p = 0.29; $l_{wthin}^2 = 5.0\%$, $l_{between}^2 = 0.0\%$, $\tau_{wthin}^2 = 0.00$, $\tau_{between}^2 = 0.00$) Between-participant Measure Mean SD Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $l_{wthin}^2 = 0.0\%$, $l_{between}^2 = 69.6\%$, $\tau_{wthin}^2 = 0.00$, $\tau_{between}^2 = 0.45$) RE Model for All Studies (df = 9, p = 0.29; $l_{wthin}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{wthin}^2 = 0.00$, $\tau_{between}^2 = 0.00$)	Azevedo et al. (2022)	VL MT	4.28	2.81	3.53	2.86		H					-0.12 [-0.59, 0.36]
Azevedo et al. (2022) VM MT 2.37 1.42 4.29 1.97 Subgroup RE Model (df = 4, p = 0.29; l_{wthin}^2 = 5.0%, $l_{between}^2$ = 0.0%, τ_{wthin}^2 = 0.00, $\tau_{between}^2$ = 0.00) Between-participant Measure Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 69.6%, τ_{wthin}^2 = 0.00, $\tau_{between}^2$ = 0.00) RE Model for All Studies (df = 9, p = 0.29; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 2.2%, τ_{wthin}^2 = 0.00, $\tau_{between}^2$ = 0.00)	Pearson et al. (2022)	Anterior thigh MT (40%)	0.24	0.29	0.21	0.32		H					-0.03 [-0.46, 0.39]
Subgroup RE Model (df = 4, p = 0.29; l_{wthin}^2 = 5.0%, $l_{between}^2$ = 0.0%, τ_{wthin}^2 = 0.00, $\tau_{between}^2$ = 0.00) Between-participant Measure Mean SD Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 -0.54 [-1.23, 0.15] -0.44 [-1.13, 0.24] -0.44 [-1.13, 0.24] -0.44 [-1.13, 0.24] -0.34 [-1.02, 0.34] Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 0.00, $\tau_{between}^2$ = 0.00) RE Model for All Studies (df = 9, p = 0.29; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 0.00, $\tau_{between}^2$ = 0.00) RE Model for All Studies (df = 9, p = 0.29; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 0.00, $\tau_{between}^2$ = 0.00) RE Model for All Studies (df = 9, p = 0.29; l_{wthin}^2 = 0.0%, $l_{between}^2$ = 0.00, $\tau_{between}^2$ = 0.00)	Azevedo et al. (2022)	RF MT	2.02	2.1	2.84	2.37				-			0.25 [-0.23, 0.73]
Between-participant Measure Mean SD Mean SD Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 -0.54 [-1.23, 0.15] Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 -0.44 [-1.13, 0.24] Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 -0.34 [-1.02, 0.34] Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 0.19 [-0.51, 0.90] Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $I_{within}^2 = 0.0\%, I_{between}^2 = 69.6\%, \tau_{within}^2 = 0.00, \tau_{between}^2 = 0.45)$ 0.25 [-1.13, 1.62] RE Model for All Studies (df = 9, p = 0.29; $I_{within}^2 = 0.0\%, I_{between}^2 = 0.00, \tau_{between}^2 = 0.00)$ 0.03 [-0.30, 0.36] Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75 0.03 [-0.30, 0.36]	Azevedo et al. (2022)	VM MT	2.37	1.42	4.29	1.97							0.30 [-0.18, 0.78]
Shibata et al. (2021) Thigh CSA (50%) 350.45 197.11 229.55 233.32 -0.54 [-1.23, 0.15] Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 -0.44 [-1.13, 0.24] Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 -0.34 [-1.02, 0.34] Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 0.19 [-0.51, 0.00] Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 1.26 [0.29, 2.23] Subgroup RE Model (df = 4, p = 0.17; $I_{within}^2 = 0.0\%, I_{between}^2 = 69.6\%, \tau_{within}^2 = 0.00, \tau_{between}^2 = 0.45)$ 0.03 [-0.30, 0.36] RE Model for All Studies (df = 9, p = 0.29; $I_{within}^2 = 0.0\%, I_{between}^2 = 0.00, \tau_{between}^2 = 0.00)$ 0.03 [-0.30, 0.36] Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75 0.00, $\tau_{within}^2 = 0.00, \tau_{between}^2 = 0.00)$ 0.03 [-0.30, 0.36]	Subgroup RE Model (df =	4, p = 0.29; I_{within}^2 = 5.0%, $I_{between}^2$	$\tau_{\rm w}^2 = 0.0\%, \ \tau_{\rm w}^2$	_{ithin} = 0.00, τ	² between = 0.00))							0.00 [-0.82, 0.83]
Shibata et al. (2021) Thigh CSA (30%) 259.64 196.91 135.68 326.66 -0.44 [-1.13, 0.24] Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 -0.34 [-1.02, 0.34] Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 0.19 [-0.51, 0.90] Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $l_{within}^2 = 0.00$, $l_{between}^2 = 69.6\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.45$) 0.25 [-1.13, 1.62] RE Model for All Studies (df = 9, p = 0.29; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.00$) 0.03 [-0.30, 0.36] Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75 0.00 0.00 0.00	Between-participant	Measure	Mean	SD	Mean	SD							
Shibata et al. (2021) Thigh CSA (70%) 379.45 223.54 292.68 262.05 -0.34 $[-1.02, 0.34]$ Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 0.19 $[-0.51, 0.90]$ Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 1.26 $[0.29, 2.23]$ Subgroup RE Model (df = 4, p = 0.17; $I_{within}^2 = 0.00, I_{between}^2 = 69.6\%, \tau_{within}^2 = 0.00, \tau_{between}^2 = 0.45)$ 0.25 $(-1.3, 1.62]$ RE Model for All Studies (df = 9, p = 0.29; $I_{within}^2 = 0.0\%, I_{between}^2 = 2.2\%, \tau_{within}^2 = 0.00, \tau_{between}^2 = 0.00)$ 0.03 $(-0.30, 0.36]$ Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75 $0.00, \tau_{between}^2 = 0.00)$ 0.03	Shibata et al. (2021)	Thigh CSA (50%)	350.45	197.11	229.55	233.32							-0.54 [-1.23, 0.15]
Kojic et al. (2021) Elbow flexor MT 3.24 2.01 3.57 1.17 Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = $0.17; l_{within}^2 = 0.00, l_{between}^2 = 69.60, r_{within}^2 = 0.00, r_{between}^2 = 0.45) 0.25 [-1.13, 1.62] RE Model for All Studies (df = 9, p = 0.29; l_{within}^2 = 0.00, l_{between}^2 = 2.2\%, r_{within}^2 = 0.00, r_{between}^2 = 0.00) 0.03 [-0.30, 0.36] Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75 0.00, r_{between}^2 = 0.00 0.00, r_{between}^2 = 0.00 $	Shibata et al. (2021)	Thigh CSA (30%)	259.64	196.91	135.68	326.66			 -{				-0.44 [-1.13, 0.24]
Pereira et al. (2016) Elbow flexor CSA 1.94 2.06 4.88 2.24 Subgroup RE Model (df = 4, p = 0.17; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 69.6\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.45$) RE Model for All Studies (df = 9, p = 0.29; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.00$) Test for Subgroup Differences: F(1, 2.68) = 0.12; df = 1, p = 0.75	Shibata et al. (2021)	Thigh CSA (70%)	379.45	223.54	292.68	262.05							-0.34 [-1.02, 0.34]
Subgroup RE Model (df = 4, p = 0.17; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 69.6\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.45$) RE Model for All Studies (df = 9, p = 0.29; $l_{within}^2 = 0.0\%$, $l_{between}^2 = 2.2\%$, $\tau_{within}^2 = 0.00$, $\tau_{between}^2 = 0.00$) Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75	Kojic et al. (2021)	Elbow flexor MT	3.24	2.01	3.57	1.17		F					0.19 [-0.51, 0.90]
RE Model for All Studies (df = 9, p = 0.29; l_{within}^2 = 0.0%, $l_{between}^2$ = 2.2%, τ_{within}^2 = 0.00, $\tau_{between}^2$ = 0.00) Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75	Pereira et al. (2016)	Elbow flexor CSA	1.94	2.06	4.88	2.24							1.26 [0.29, 2.23]
Test for Subgroup Differences: F(1, 2.68) = 0.12, df = 1, p = 0.75	Subgroup RE Model (df =	4, p = 0.17; I_{within}^2 = 0.0%, $I_{between}^2$, = 69.6% , τ	$\frac{2}{\text{within}} = 0.00,$	$\tau_{between}^2 = 0.4$	45)	······					ł	0.25 [-1.13, 1.62]
-3 -2 -1 0 1 2 3			etween = 2.2%	b, $\tau_{\text{within}}^2 = 0.0$	00, $\tau_{between}^2 =$	0.00)							0.03 [-0.30, 0.36]
						-3	-2	-1	0	1	2	3	

335

Fig. 4 Forest plot for pooled muscle hypertrophy analysis, including subgroup and moderator
 analysis for study design. The red lines represent the lower and upper bounds of our region of
 practical equivalence (±0.28). *Cl* confidence interval, *SD* standard deviation, *CSA* Cross-sectional
 area, *MT* muscle thickness, *VL* vastus lateralis, *RF* rectus femoris, *VM* vastus medialis

340 **3.4.3 Countermovement jump height**

The pooled analysis for CMJ revealed that the average effect most compatible with our data, given

our statistical model, was a large effect favouring FEG with poor precision (Figure 5). The effect

size ranged from large effects favouring FEG to small effects favouring SEG (-0.73 [90% Cl = -1.34,

 $-0.12, 90\% \text{ PI} = -1.34, -0.12; 95\% \text{ CI} = -1.64, 0.17; 95\% \text{ PI} = -1.64, 0.17], p = 0.07, l^2_{\text{within}} = 0\%,$

345 $I_{between}^2 = 0\%$, $\tau_{within}^2 < 0.01$, $\tau_{between}^2 < 0.01$). Considering our ROPE (±0.11), the 90% CI, and 90% PI,

there is evidence to support that FEG enhances CMJ improvement by a practically worthwhile

347 degree, compared to SEG.



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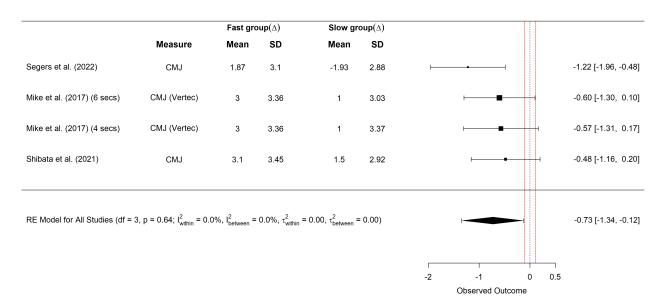
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Author(s) and Year

Estimate [90% CI]



348

Fig. 5 Forest plot for pooled countermovement jump analysis. The red lines represent the lower
 and upper bounds of our region of practical equivalence (±0.11). *Cl* confidence interval, *SD*

351 standard deviation, CMJ Countermovement Jump

352

353 **3.4.4 Sensitivity analyses**

354 The results for maximal strength and hypertrophy were both robust to sensitivity analysis with a lower and higher imputed sampling error correlation co-efficient ($\rho = 0.4$ and 0.8) (see full 355 sensitivity analyses in Supplementary file 5). Hat values were not violated for maximal strength or 356 357 hypertrophy, nor Cook's distance for maximal strength, but a potential outlier was identified as violating the threshold for Cook's distance for hypertrophy. Removing this study [56] from the 358 359 analysis did not change the interpretation of the model estimate (practically not worthwhile effect size favouring SEG; from g = 0.03 to 0.16) but increased its' uncertainty (95% CI from [-0.43, 0.48] 360 361 to [-0.71, 1.03].



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Table 2 Summary of findings

Outcome (<i>n</i> , <i>k</i>)	Hedge's <i>g</i> (90% CI)	<i>p</i> -value (95% CI)	$I^2_{\rm within}$, $I^2_{\rm between}$	Certainty of evidence
	[90% PI]	[95% PI]	$[\tau^2_{within}, \tau^2_{between}]$	(GRADE)
Strength				
Pooled (<i>n</i> = 148, <i>k</i> = 8)	0.18 (-0.27, 0.63)	0.48 (-0.39, 0.74)	0.0%, 65.8%	$\oplus \oplus \ominus \ominus$
Follow-up: 4-12 weeks	[-0.96, 1.31]	[-1.24, 1.60]	[< 0.01, 0.30]	Low ^{b,f,h}
Trained (<i>n</i> = 77, <i>k</i> = 4)	0.34 (0.07, 0.60)	0.06 (-0.04, 0.72)	0.0%, 0.0%	$\oplus \oplus \oplus \ominus$
Follow-up: 4-12 weeks	[0.07, 0.60]	[-0.04, 0.72]	[<0.01, <0.01]	Moderate ^e
Untrained ($n = 71, k = 4$)	-0.03 (-1.24, 1.18)	0.95 (-1.68, 1.61)	0.0%, 84.6%	$\oplus \ominus \ominus \ominus$
Follow-up: 6-12 weeks	[-2.60, 2.53]	[-3.50, 3.43]	[<0.01, 0.92]	Very low ^{c,g}
Multi-joint (<i>n</i> = 93, <i>k</i> = 4)	-0.11 (-1.08, 0.86)	0.80 (-1.43, 1.21)	0.0%, 73.3%	$\oplus \ominus \ominus \ominus$
Follow-up: 4-12 weeks	[-2.07, 1.85]	[-2.76, 2.54]	[<0.01, 0.52]	Very low ^{c,g}
Single-joint ($n = 74, k = 4$)	0.40 (-0.22, 1.03)	0.23 (-0.47, 1.27)	24.9%, 24.9%	$\oplus \ominus \ominus \ominus$
Follow-up: 7-12 weeks	[-0.68, 1.48]	[-1.10, 1.90]	[0.06, 0.06]	Very low ^{c,f}
Sets-to-failure (<i>n = 64, k = 4</i>)	0.10 (-1.21, 1.41)	0.87 (-1.67, 1.87)	42.6%, 42.6%	$\oplus \ominus \ominus \ominus$
Follow-up: 7-12 weeks	[-2.64, 2.84]	[-3.60, 3.81]	[0.52, 0.52]	Very low ^{d,g}

All authors have read and approved this version of the manuscript. This article was last modified on Month XX, YEAR.

Authors X @*xtwitter* and Y @*ytwitter* can be reached on Twitter.

Volume-load (<i>n = 84, k = 4</i>)	0.25 (0.04, 0.45)	0.07 (-0.03, 0.53)	0.0%, 0.0%	$\oplus \oplus \oplus \ominus$
Follow-up: 4-12 weeks	[0.04, 0.45]	[-0.03, 0.53]	[<0.01, <0.01]	Moderate ^e
Between-participants (<i>n = 125, k = 6</i>)	0.21 (-0.50, 0.93)	0.58 (-0.70, 1.13)	0.0%, 73.4%	$\oplus \ominus \ominus \ominus$
Follow-up: 4-12 weeks	[-1.46, 1.88]	[-1.92, 2.34]	[<0.01, 0.56]	Very low ^{c,g}
Within-participants ($n = 23, k = 2$)	0.11 (-0.52, 0.75)	0.47 (-1.16, 1.39)	0.0%, 0.0%	$\oplus \ominus \ominus \ominus$
Follow-up: 8 weeks	[-0.52, 0.75]	[-1.16, 1.39]	[<0.01, <0.01]	Very low ^g
Hypertrophy				
Pooled $(n = 77, k = 5)$	0.03 (-0.30, 0.36)	0.86 (-0.42, 0.48)	0.0%, 2.2%	$\oplus \ominus \ominus \ominus$
Follow-up: 6-12 weeks	[-0.32, 0.38]	[-0.45, 0.51]	[<0.01, <0.01]	Very low ^{c,f}
Trained ($n = 25, k = 2$)	0.46 (-3.84, 4.77)	0.62 (8.20, 9.13)	0.0%, 87.5%	$\oplus \ominus \ominus \ominus$
Follow-up: 8-12 weeks	[-6.49, 7.42]	[-13.54, 14.47]	[<0.01, 0.75]	Very low ^{a,c,g}
Untrained ($n = 52, k = 3$)	- 0.01 [-0.62, 0.61]	0.97 (-0.97, 0.96)	1.2%, 4.3%	$\oplus \ominus \ominus \ominus$
Follow-up: 6-8 weeks	[-0.68, 0.67]	[-1.06, 1.05]	[<0.01, <0.01]	Very low ^{c,g}
Arm (<i>n = 32, k = 2</i>)	0.29 (-0.82, 1.40)	0.51 (-1.39, 1.97)	0.0%, 66.4%	$\oplus \ominus \ominus \ominus$
Follow-up: 7-12 weeks	[-1.57, 2.16]	[-2.53, 3.11]	[<0.01, 0.23]	Very low ^{a,c,g}
Thigh (<i>n</i> = 45, <i>k</i> = 3)	-0.09 (-1.89, 1.71)	0.80 (-3.73, 3.54)	1.3%, 38.5%	$\oplus \ominus \ominus \ominus$
Follow-up: 6-8 weeks	[-2.60, 2.42]	[-5.14, 4.97]	[<0.01, 0.08]	Very low ^{c,g}
Between-participants (<i>n</i> = 54, <i>k</i> = 3)	0.25 (-1.13, 1.62)	0.65 (-1.79, 2.29)	0.0%, 69.6%	$\oplus \ominus \ominus \ominus$
Follow-up: 6-12 weeks	[-2.18, 2.67]	[-3.34, 3.84]	[<0.01, 0.45]	Very low ^{d,g}

Within-participants $(n = 23, k = 2)$	0.00 (-0.82, 0.83)	0.98 (-1.66, 1.67)	5.0%, 0.0%	$\oplus \Theta \Theta \Theta$
Follow-up: 8 weeks	[-0.91, 0.92]	[-1.84, 1.85]	[<0.01, <0.01]	Very low ^g
СМЈ				
Pooled (<i>n</i> = 74, <i>k</i> = 3)	-0.73 (-1.34, -0.12)	0.07 (-1.64, 0.17)	0.0%, 0.0%	$\oplus \oplus \oplus \ominus$
Follow-up: 4-6 weeks	[-1.34, -0.12]	[-1.64, 0.17]	[<0.01, <0.01]	Moderate ^{f,i}

Explanations

^a Serious risk of bias due to allocation concealment and lack of blinding.

^b Serious inconsistency (moderate heterogeneity $I^2 > 50\%$ and point estimates vary considerably), that may be explained by training status.

^c Serious unexplained inconsistency (point estimates vary considerably).

^d Very serious unexplained inconsistency (large point estimates in each direction).

^e Serious imprecision (95% CI crosses one equivalence bound).

^f Very serious imprecision (95% crosses both equivalence bounds)

^g Extremely serious imprecision (95% CI crosses both equivalence bounds with large effects in both directions).

^h Plausible residual confounder of training status.

ⁱ Presence of large effects.

CI confidence interval, PI prediction interval, SD standard deviation, CMJ countermovement

jump, *k* number of studies, *n* number of participants

Table 3 Results from moderator analyses	

	Hedge's <i>g</i> [90% CI]	<i>p</i> -value	95% CI
Strength			
Training status	-0.42 [-1.37, 0.53]	0.42	-1.62, 0.78
Exercise type	0.55 [-0.40, 1.50]	0.31	-0.65, 1.75
Volume matching	0.17 [-0.88, 1.24]	0.76	-1.16, 1.52
Study design	-0.11 [-1.20, 0.99]	0.80	-1.73, 1.52
Hypertrophy			
Training status	-0.33 [-2.17, 1.51]	0.66	-2.98, 2.32
Muscle group	-0.36 [-1.53, 0.81]	0.49	-2.01, 1.29
Study design	-0.17 [-1.31, 0.98]	0.75	-1.74, 1.41

Cl confidence interval



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4. Discussion

The aim of this systematic review was to quantitatively explore the effects of manipulating eccentric tempo duration on indices of muscular performance and hypertrophy. The main results from the meta-analysis indicated that faster eccentric tempo durations, with moderate certainty of evidence, result in large and practically worthwhile increases in CMJ height following RT. For strength and hypertrophy, results were generally too uncertain to statistically support or reject the presence or absence of a practically worthwhile impact of eccentric tempo manipulation, highlighting the need for further research. Notably, when participants are trained or when volume-load is matched, slower eccentric tempo may, with moderate certainty of evidence, lead to practically similar or higher strength gains compared to faster eccentrics.

Our results indicate that faster eccentric phase durations lead to larger improvements in CMJ across 4-6 weeks of squat training, suggesting that prolonging the eccentric phase duration, at least in the short-term, may not maximise ballistic performance. This might be a result of the reduced residual force enhancement from the longer eccentric phase [16,58], possibly attenuating the stretch-shortening cycle (SSC) specific training adaptations associated with faster eccentrics. Interestingly, while Shibata and colleagues [53] did report larger CMJ effects after faster eccentric phase durations (1.5 cm [4.2%] vs. 3.1 cm [8.4%]), they also found larger effects for squat jump height (i.e., without an SSC) after slower eccentric phase durations (2.4 cm [7.2%] vs. 1.9 cm [5.3%]). While these results were not statistically different, others also found larger effects in non-SSC performance tests by reducing residual force enhancement (i.e., by imposing a pause between the eccentric and concentric phase during squat training [59]). Therefore, modifying residual force enhancement via tempo alteration to more precisely improve specific strength and conditioning outcomes may be viable. However, more research exploring tempo manipulation on SSC and non-SSC performance is needed.

For maximal strength, longer eccentric phase durations led to practically similar or larger improvements in than faster eccentric phase durations in trained participants and when

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volume-load was matched. It should be recognised that decisions regarding the ROPE are context-dependent [60], and we chose these values as they were likely representative of typical study participants. However, it could be argued that given the low real-world cost of tempo manipulation, any measurable effect may be relevant, particularly in highly trained athletes. For example, by converting our trained subgroup 90% CI into percentages ($\Delta M_{\%} = \Delta SD_{\%} \times ES$), using the only study that employed free-weight back squats in trained participants [54], we see that prolonging the eccentric enhances strength gains by an additional ~0.4-3.0% over 4-12 weeks compared to doing faster eccentrics. We therefore urge readers to interpret results based on what they would deem relevant in their practice.

Some explanations for why slower eccentrics may enhance strength gains may be that they i) lead to enhanced neural adaptations, ii) produce similar or larger training stimuli, and/or iii) incur less fatigue. First, a recent systematic review found tempo-controlled RT may enhance neural adaptation and task-specific motor learning, compared to self-paced RT [61], likely due to increased cognitive effort needed to meet the prescribed tempo. Given we only found equal or higher strength gains for trained participants, it may be that self-paced or faster eccentric durations provide sufficient motor learning for less trained populations; however, as skill increases, additional movement challenge is needed to progress motor skill, as suggested elsewhere [62]. However, the interaction between exercise execution/selection and training status is relatively unexplored.

Second, by prolonging the eccentric phase, total and eccentric time under tension increase [53,55,57], which typically leads to lower absolute loads or less overall repetitions completed when either repetitions or loads are kept constant, respectively, at the same proximity-to-failure [14,16,53]. Conversely, when repetitions per set at a submaximal load are fixed, slower eccentric tempos lead to closer proximities to failure [56], suggesting that prolonging the eccentric phase makes each repetition more strenuous. This might explain why Shibata and colleagues [53] observed large effects favouring fast eccentrics (-1.40), relative to the other squat studies in trained participants (0.37-0.57) [52,54] and the remaining studies in untrained (-0.09-1.27) [51,55,57]. These participants performed 3 sets to failure at 75% of 1RM, which, on average, had participants squatting for 42-78 sec per set, ultimately causing a large drop in completed repetitions in the SEG across six weeks. The other squat study participants only performed 3-6 repetitions per set at 70-85% of 1RM [52,54], did not reach failure when performing multi-joint exercises at higher repetitions [51] or used isolation exercises when

reaching muscular failure [55,57], possibly allowing participants to perform each set with less cardiovascular strain and, thus, not interfering with the training stimulus. This might also explain why the limited data on very long eccentric tempo durations exhibit no signs of a dose-response gradient (ES: 4s = 1.68, vs. 6s = 1.38 [52]; 4s = 1.69, vs. 10s = 1.27 [63]), possibly due to performance declining as eccentric tempo durations increase [15,16]. As such, slower eccentrics may allow trainees to experience similar training stimuli with lower volume-loads or improve the stimulus with the same volume-load (see subgroup analyses for matching method), if eccentric duration is not taken to extremes.

Third, some studies [52,64], but not all [54], report that prolonging eccentric tempo, despite leading to acute performance decrements, may result in less neuromuscular fatigue and delayed onset muscle soreness after training, suggesting slower eccentric training allows trainees to reach similar or higher training stimuli with lower or similar volume-loads at a lower fatigue cost. Therefore, eccentric tempo manipulation may enhance strength gains in trained participants due a combination of factors possibly related to increased motor learning, and improved training stimulus with lower fatigue. However, successfully implementing eccentric tempo manipulation for maximal strength likely depends on striking a balance between eccentric phase duration and volume and load to minimise unnecessary performance decrements by limiting excessive muscular and/or cardiovascular fatigue. Future research should investigate the impact of how training parameters are matched and how this impacts the effect of eccentric tempo manipulation.

For muscle hypertrophy, results were too uncertain to infer the absence or presence of practically worthwhile effects. While point estimates of our subgroup analyses generally followed the trends from our strength results, implying that a possible reason for improved strength could be greater rates of muscle gain in trained participants, these results were very uncertain, and more research is needed. No studies explored muscle architecture, and two [53,56] that explored regional hypertrophy found diverging results. As such, research exploring the effects of eccentric tempo manipulation on muscle morphology is warranted. Ultimately, while including an eccentric phase is important for maximising muscle hypertrophy [11], whether its duration affects muscle hypertrophy by a practically worthwhile degree cannot be currently determined.

This systematic review with meta-analysis has several limitations. First, the included number of studies and participants per study was low. This was accounted for in our effect size calculations and robust variance estimations, leading to wide confidence intervals, which, combined with our interpretative lens, lead to more cautious conclusions based on the uncertainty of results. Second, some subgroup analyses were not pre-planned and should therefore be considered exploratory. Given the point estimates we found, we urge researchers to conduct studies exploring the impact of training status, how volume was matched between groups, impact of relative-load and exercise selection on the effect of eccentric tempo manipulation. Lastly, given the different adaptations from slow(er) and fast(er) eccentric tempos, it is unclear whether a combined approach would be more suitable to concurrently enhance multiple measures of performance, or possibly achieve a synergistic effect.

5. Conclusion

In conclusion, with moderate certainty, faster eccentrics are better for improving CMJ height, while relatively longer eccentric phase durations produce similar or larger strength gains in trained participants and under volume-load matched conditions. Due to very low certainty of evidence, the absence or presence of whether a practically worthwhile effect of eccentric tempo manipulation for muscle hypertrophy cannot be confidently inferred. More research is needed to explore the impact of eccentric tempo duration on SSC vs. non-SSC ballistic performance outcomes, maximal strength, and muscle morphology. Future research should aim to improve the certainty of inferences and examine the interactions with volume matching, training status, relative load, concurrent approaches and responses across different muscle groups and exercises.

6. Practical applications

Coaches and athletes may manipulate eccentric phase duration depending on their goal. Faster eccentric tempos are likely better suited for improving ballistic SSC performance, while slower eccentric tempos may be used to achieve similar or greater increases in non-SSC ballistic performance and maximal strength, in trained participants. The dose, exercise selection, athlete needs, and competition schedule should be considered, such that specific tempos allow for maximal development of the desired outcome, without hindering specific practice during important parts of the season. Regardless of goal, prolonging eccentric phases can serve as a load and fatigue management tool by allowing trainees to i) increase exertion levels with the same repetitions and load, ii) obtain a similar training stimulus with less absolute volume-load completed, and iii) reduce overall recovery demands from training. Therefore, worthy of specific note, is that in cases where discomfort or pain is associated with higher load training, slower eccentric durations may be a useful method to maintain strength adaptations with lower loads. Based on practical experience and limited evidence, we recommend: i) the eccentric phase should not be prolonged excessively (i.e., 3-5 seconds seems reasonable), ii) using low to moderate repetitions (1-6 repetitions) when employing slower eccentrics for multi-joint exercises, and iii) if using slower eccentric durations for higher repetitions to or near muscular failure, consider doing so with isolation exercises. This is to avoid excessive cardiovascular and metabolic fatigue that may impair progress and decrease the lifters' willingness to perform the tempo as prescribed.

Contributions

Both authors contributed to study conception, design, and literature search. Data extraction was performed by CHA. Data analysis and visualisation was performed by AK. The first draft was written by CHA and both authors provided revisions. Both authors read and approved the final manuscript.

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Data and Supplementary Material Accessibility

All supplementary materials, including statistical code and dataset, can be found at Open Science Framework (<u>https://osf.io/s6uqn/</u>).

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