



Community-based postural control assessment in autistic individuals indicates a similar, but delayed, trajectory compared to neurotypical individuals

For correspondence:
millerHL@umich.edu

Nicholas E. Fears, Ph.D.^{1,2}; Gabriela M. Sherrod, B.S.^{1,3}; Tylan N. Templin, M.S.^{1,4}; Nicoleta L. Bugnariu, PT, Ph.D., MBA^{1,5}; Rita M. Patterson, Ph.D.⁶; Haylie L. Miller, Ph.D.^{1,2}

1University of North Texas Health Science Center, School of Health Professions, 3500 Camp Bowie Blvd., Fort Worth, TX, 76109, USA; 2University of Michigan, 830 N. University Ave., Ann Arbor, Michigan, 48170, USA; 3University of Alabama at Birmingham, 1720 University Blvd., Birmingham, AL, 35294, USA; 4Southwest Research Institute, 6220 Culebra Rd., San Antonio, TX, 78238, USA; 5University of the Pacific, School of Health Sciences, 155 Fifth St., San Francisco, CA, 94103, USA; 6University of North Texas Health Science Center, Texas College of Osteopathic Medicine, 3500 Camp Bowie Blvd., Fort Worth, TX, 76109, USA

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Authors NEF @*NickFears* and HLM @*haylie_miller* can be reached on Twitter.

ABSTRACT

Autistic individuals exhibit significant sensorimotor difficulties. Postural stability and control are foundational motor skills for successfully performing many activities of daily living. In neurotypical development, postural stability and control develop throughout childhood and adolescence. In autistic development, previous studies have focused primarily on individual age groups (e.g., childhood, adolescence, adulthood) or only controlled for age using age-matching. Here, we examined the age trajectories of postural stability and control in autism from childhood through adolescents using standardized clinical assessments. In study 1, we tested the postural stability of autistic (n=27) and neurotypical (n=41) children, adolescents, and young adults aged 7-20 years during quiet standing on a force plate in three visual conditions: Eyes Open (EO), Eyes Closed (EC), and eyes open with the head in a translucent dome (Dome). Postural sway variability decreased as age increased for both groups, but autistic participants showed greater variability than neurotypical participants across age. In study 2, we tested autistic (n=21) and neurotypical (n=32) children and adolescents aged 7-16 years during a dynamic postural control task with 9 targets. Postural control efficiency increased as age increased for both groups, but autistic participants were less efficient compared to neurotypical participants across age. Together, these results indicate that autistic individuals have a similar age trajectory for postural stability and control compared to neurotypical individuals, but have lower postural stability and control overall.

INTRODUCTION

Motor differences are highly-prevalent in Autism Spectrum Disorder (autism/autistic), with estimates as high as 90% (Green et al., 2009; Hilton, Zhang, Whilte, Klohr, & Constantino, 2012; Miller, et al., 2021), and persistent across the lifespan (Bhat, Landa, & Galloway, 2011). In early childhood, autistic children exhibit motor delays (Davidovitch, Stein, Koren, & Friedman, 2018; Fulceri et al., 2019) and lower postural stability (Leezenbaum & Iverson, 2019). In the school years, autistic children often have lower scores on standardized assessments of gross- and fine-motor skills (Green et al., 2009; Hilton et al., 2012; Kaur, Srinivasan, & Bhat, 2018). As adults, autistic individuals show a wide range of differences in motor skills, from reaching (Campioni, Piazza, Villa, & Molteni, 2016; Glazebrook, Elliott, & Lyons, 2006) to postural stability (Domas, McKenna, & Murphy, 2016; Lim et al., 2018). Further, these differences in motor skills are related to differences in functional abilities (Licari et al., 2019; Travers et al., 2017). Despite clear motor skill differences and their effect on functional abilities across the lifespan in autism, there has been relatively little work to characterize the age trajectory (i.e., change across age,

maturation, and experience) of specific domains of motor ability, such as postural stability and postural control.

Clinical relevance of postural stability and sensory reweighting

Decreased postural stability can affect the performance of simple tasks like quiet standing, which is heavily reliant on sensorimotor integration (Cuisinier et al., 2011; Shumway-Cook & Woollacott, 1985; Sparto et al., 2006; Woollacott et al., 1987). Autistic individuals exhibit lower postural stability during quiet standing (for review, see Lim, Partridge, Girdler, & Morris, 2017). Additionally, neuroimaging studies have demonstrated atypical sensory-motor neural connectivity in autism (Hanaie et al., 2013; Hau et al., 2021; Linke et al., 2020; Mostofsky et al., 2009; Oldehinkel et al., 2019; Thompson et al., 2017; Travers et al., 2015; Unruh et al., 2019; Wang et al., 2019). Further, these differences in neural connectivity have been shown to be related to motor abilities in autistic individuals (Hanaie et al., 2013; Thompson et al., 2017; Travers et al., 2015; Unruh et al., 2019; Wang et al., 2019).

Prior studies of sensory reweighting in autistic children and adults have produced mixed results regarding the level of reliance on vision to maintain static postural stability, with some studies indicating an over-reliance on vision and others reporting no difference (Lim et al., 2017). Kohen-Raz et al. (1992) reported reduced anteroposterior stability in autistic participants aged 6-20 years during quiet standing under differing visual and proprioceptive conditions requiring sensory reweighting. Minschew, Sung, Jones, and Furman (2004) examined postural stability development in autistic children and adults in the anterior-posterior direction under different sensory conditions. Their findings indicated differences in postural stability between autistic and neurotypical individuals across age, but they did not address potential differences in medial-lateral postural stability, or in the overall amount of postural sway exhibited under different sensory conditions. Together, these studies indicate that sensorimotor functioning in autistic individuals is different from neurotypical individuals and support the need for further investigation into the development of sensorimotor integration for postural stability in autistic individuals. A particular focus on medial-lateral stability is necessary, given that it is a stronger predictor of fall risk compared to anterior-posterior stability (Piirtola & Era, 2006). It is also a useful measure of change over time, given the clear developmental trajectory that can be observed across childhood and into adolescence and adulthood (Blanchet et al., 2019).

Clinical relevance of dynamic postural control

Dynamic postural control is necessary for activities of daily living including dressing and carrying objects (Haddad, Rietdyk, Claxton, & Huber, 2013), participation in physical activity (Stodden et al., 2008), and mobility (Le Mouel & Brette, 2017). A person's *limit of stability*, or the distance that they are able to move their center of mass outside of their base of support without taking a compensatory step to regain balance, impacts their ability to perform functional movements. Dynamic postural control has been identified as a strong predictor of fall risk across multiple populations (Holbein-Jenny et al., 2007; Swanenburg, de Bruin, Uebelhart, & Mulder, 2010; Sun, Hsieh, & Sosnoff, 2019), and difficulty engaging in well-controlled weight shifts has been implicated as a precursor of falling events (Robinovitch et al., 2013). Prior literature suggests that the neuromotor mechanisms of dynamic postural control differ from those of static postural control, and that dynamic instability may be a stronger driver of injury (e.g., Granacher & Gollhofer, 2011). Given the clinical relevance of dynamic postural control and the impact of limits of stability on functional movement, it is surprising that there is substantially less research on dynamic postural control compared to static postural stability in autism.

In the few studies on dynamic postural control in autism that have been reported, autistic individuals have exhibited less efficient dynamic postural control compared to neurotypical individuals (Bojanek, Wang, White, & Mosconi, 2020; Fournier et al., 2010; Miller, Caçola, Sherrod, Patterson, & Bugnariu, 2019; Wang et al., 2016). One metric of dynamic postural control efficiency is the directness of the path taken between a starting position and a target location during leaning. Autistic individuals use longer path lengths when leaning in the anteroposterior and mediolateral directions compared to neurotypical individuals (Wang et al., 2016). This finding is particularly suggestive of inefficiency given that in the same study, the limit of the length and width of postural stability was similar between autistic and neurotypical participants (Wang et al., 2016). This research demonstrates that dynamic postural control is different in autistic individuals and warrants further study.

While many dynamic postural control tasks require a large amount of space (e.g., gait analysis), assessments of a person's limit of stability can be administered using the same equipment and space as quiet standing. This reduces barriers to the feasibility of administering it as part of a postural stability assessment battery that yields more comprehensive results than standard clinical assessments (e.g., Romberg's Test). By removing barriers to assessments of postural control, we can diversify the individuals included in our research studies and improve their generalizability.

Improving sample diversity and community-based assessments

The feasibility of conducting static and dynamic postural control assessments using computerized posturography with autistic individuals in community settings has not been established. While these assessments are common in some clinics (e.g., physical therapy, neurology), they are not often used outside of research labs or clinics, especially in autism. However, studies of other neuromotor disorders have demonstrated the efficacy of computerized posturography efficacy in detecting postural stability problems with higher sensitivity than common clinical tests like Romberg's Test, even among minimally-impaired individuals (Melillo et al., 2017). Given the potential for "white coat effects" on performance in clinics (Cleworth, Inglis, & Carpenter, 2018; Geh et al., 2011), which could be more pronounced for autistic people (Gillis et al., 2009), there is a need to establish the feasibility of these assessments in detecting balance problems of autistic individuals in community settings. In addition, the utility of standardized assessments across a wide variety of settings and populations is an important consideration, given the historic limitation of autism research with respect to sample diversity and complexity of lab- and clinic-based assessment protocols.

Autism researchers have long relied primarily on white, middle-class, and highly educated families to participate in our research studies (West et al., 2016). Across 408 studies, West and colleagues (2016) found that of all autism research participants, between 2.1% and 6.8% identify as Black and between 0.8% and 2.5% identified as Hispanic. This has likely contributed to racial and ethnic disparities in autism diagnostic instruments (Harrison, Long, Tommet, & Jones, 2017), likelihood of diagnosis (Mandell et al., 2009), and use of services (Smith et al., 2020; Yingling, Bell, & Hock, 2019). This has led to a number of calls for improving the diversity in our samples by reducing barriers to participation in our studies (Jones & Mandell, 2020).

In the current studies, we partnered with local community organizations, used portable technology, and short, easy to understand study protocols translated in English and Spanish to include families that are often excluded from research (Sankare et al., 2015). Using portable technology and a short study protocol, we were able to meet families in locations close to where they live, work, and play. We recruited and tested participants in local schools, museums, community centers, public libraries, and at autism-focused community events. This played a substantial role in recruiting a much more diverse sample compared to prior studies, with more than 25% identifying as Hispanic and more than 10% identifying as Black. By including a more diverse sample, we hope to improve the generalizability of our findings beyond those typically included in autism research studies.

Current studies

The current studies examine age trajectories of static postural stability (Study 1) and dynamic postural control (Study 2). We used an established, portable, clinical assessment tool (i.e., Biodex Biosway) and a community-based recruitment and testing protocol to assess diverse samples of children, adolescents, and young adults. We performed two standardized postural control tasks, the Clinical Test of Sensory Integration and Balance (CTSIB) and a limits of stability (LOS) task. CTSIB and LOS can be administered quickly (<15 minutes) and with limited need for space. This makes them excellent for use in community settings. The goal of our community-based recruitment strategy was to lower potential barriers to participation in our science and improve our understanding of the autism community. By doing so, we were able to increase participation of individuals from races and ethnicities that are often underrepresented in autism research. Together, these two studies yielded excellent data for understanding age trajectories of postural stability and postural control in a more more generalizable sample of autistic individuals.

STUDY 1

Despite well-documented differences in postural stability and sensory reweighting in autism, to our knowledge, only one study (Minshew et al., 2004) has specifically assessed their age trajectory. This is in stark contrast to the neurotypical literature, where the development of postural stability is well-characterized across childhood and adolescence (e.g., Assaiante et al., 2005; Bair et al., 2007; Verbecque, Vereek, & Halleman, 2016). In this study, we examined the *magnitude* of postural sway and *variability* in postural sway in autistic children and adolescents. We used these measures to assess the development of postural stability and sensory reweighting among autistic and neurotypical children and adolescents. Based on previous findings (Minshew et al., 2004), we predicted that the age trajectory of sway variability would be similar in autistic and neurotypical individuals, but that autistic individuals would have consistently greater sway variability (indicating less overall postural stability) than their neurotypical peers. Additionally, we predicted that limiting the availability of visual context would have a greater effect on sway variability for autistic participants than neurotypical participants, reflecting atypical sensory reweighting.

Participants

We tested autistic ($n=27$, Male=22, Female=5; $M_{age}=12.44$ years, $SD_{age}=3.18$ years, $range=8.20-20.59$ years) and neurotypical ($n=41$, Male=16, Female=25; $M_{age}=10.89$ years, $SD_{age}=3.50$ years, $range=7.10-20.90$ years) children and adolescents. Participants reported their

race as American Indian/Alaska Native (1.49%), Asian (4.56%), Black/African American (14.87%), or White (74.75%). Three participants declined to report their race (4.45%). A total of 25.25% of participants reported being of Hispanic ethnicity. Autistic participants had a prior diagnosis of autism or Asperger's syndrome from an educational or healthcare professional (e.g., school psychologist, clinical psychologist, physician) according to DSM-IV or DSM-5 criteria. Diagnosis, age at diagnosis, and source of diagnosis were reported by parents or self-advocates. Because one purpose of this study was to demonstrate the feasibility of a short community-based protocol for assessment of postural control, the research team did not independently confirm each participant's diagnosis, as this would have required a minimum of one hour. However, prior work suggests 90% concordance between reported community diagnosis and consensus diagnosis by a research team for individuals with a diagnosis of autism or Asperger's syndrome (Hausman-Kedem, et al., 2018). We excluded participants who could not follow 2-step directions (e.g., "Stand here, look there."), were currently taking benzodiazepines, had consumed caffeine, tobacco, or alcohol in the previous 2 hours, or weighed less than 50 lbs (22.68 kg). This study was approved by the Institutional Review Board at the University of North Texas Health Science Center. Prior to participation, all guardians gave informed consent, and all minor participants gave assent.

Clinical Test for Sensory Integration in Balance

The Clinical Test for Sensory Integration in Balance (CTSIB) is used to assess the ability to appropriately reweight sensory information to maintain standing balance under different visual conditions (Cohen, Blatchly, & Gomash, 1993; Shumway-Cook & Horak, 1986). Participants stood on the hard surface of a portable 20Hz force plate (BioSway, Biodex Corp.) and remained still for 30-second intervals in each of the following conditions: eyes open (EO), eyes closed (EC), and eyes open with a translucent paper sphere placed around the participant's head (Dome). The EO condition enabled assessment of static postural stability when all relevant sensory inputs were available and reliable, and when a visual target was displayed at approximately eye height on a screen in front of the participant. The EC condition enabled measurement of postural stability when participants did not have visual input available, requiring greater reliance on proprioceptive and vestibular input. In the Dome condition, participants had visual input, but this input lacked functional context. Participants had to maintain stability without the ability to fixate on visuospatial cues from the environment, which would typically be used by both autistic (Molloy et al., 2013) and neurotypical people (Schärli et al., 2012) to support stability.

Traditionally, the CTSIB tests each of the visual conditions on a firm surface and on compliant foam (Cohen et al., 1993; Shumway-Cook & Horak, 1986). In the present study, we administered only the firm surface condition. Each participant's foot position was standardized to the center of the force plate based on their height; any deviation from the original position was corrected prior to the start of the next condition. Individual trials in which participants did

not keep their feet firmly on the surface of the force plate (e.g., took a step, raised their heels, moved their feet) were discarded and, whenever possible, readministered after correcting foot placement.

Data Analyses

The BioSway system calculates two standardized postural stability indices: *Stability Index* and *Sway Index*. We refer to these as *sway magnitude* and *sway variability*, respectively, as this more accurately reflects the nature of these indices and their particular contributions to postural stability. These indices are based on a participant's *sway angle* calculated in both the X and Y directions. Sway angle is calculated by the BioSway software as the magnitude of the distance between the participant's center of pressure and the center of the force plate, divided by 55% of the height of the individual (the estimated height of their center of mass) and scaled by a factor of 250.

Sway magnitude is the participant's mean angular displacement from center during the trial, with higher values indicating greater displacement (Supplementary Material 1). Sway variability is the root mean square distance of the participant's angular displacement from center (Supplementary Material 2). The higher the sway variability, the more unsteady the participant was across the duration of the trial.

Using generalized linear mixed effects models, we regressed sway magnitude and sway variability on fixed factors of group (autism, neurotypical), age (continuous), and condition (EO, EC, Dome) with a random intercept by participant (Bates, Machler, Bolker, & Walker, 2015). We conducted χ^2 -tests for fixed effects of generalized linear and linear mixed-effects models (Fox & Weisberg, 2019) and post hoc *t*-tests on estimated marginal means using Tukey's method for multiple comparisons (Lenth, 2020). Estimated marginal means and standard errors are reported in response-scale, and β -weights are reported in link-scale.

RESULTS

Sway magnitude

A generalized linear mixed-effects model with a Gamma distribution and a log link regressing sway magnitude onto group, age, and condition indicated differences by condition, but not by group, age, or their interactions. There was a significant main effect of condition ($\chi^2_2=13.12, p=.001$, Figure 1). Participants showed greater sway magnitude in the Dome ($M=2.27, SE=0.19, p=.001$) condition compared to the EO condition ($M=1.77, SE=0.15$). Sway magnitude was not significantly different between the EO and EC conditions ($M=2.07, SE=0.18, p=.061$) or the EC and Dome conditions ($p=.361$).

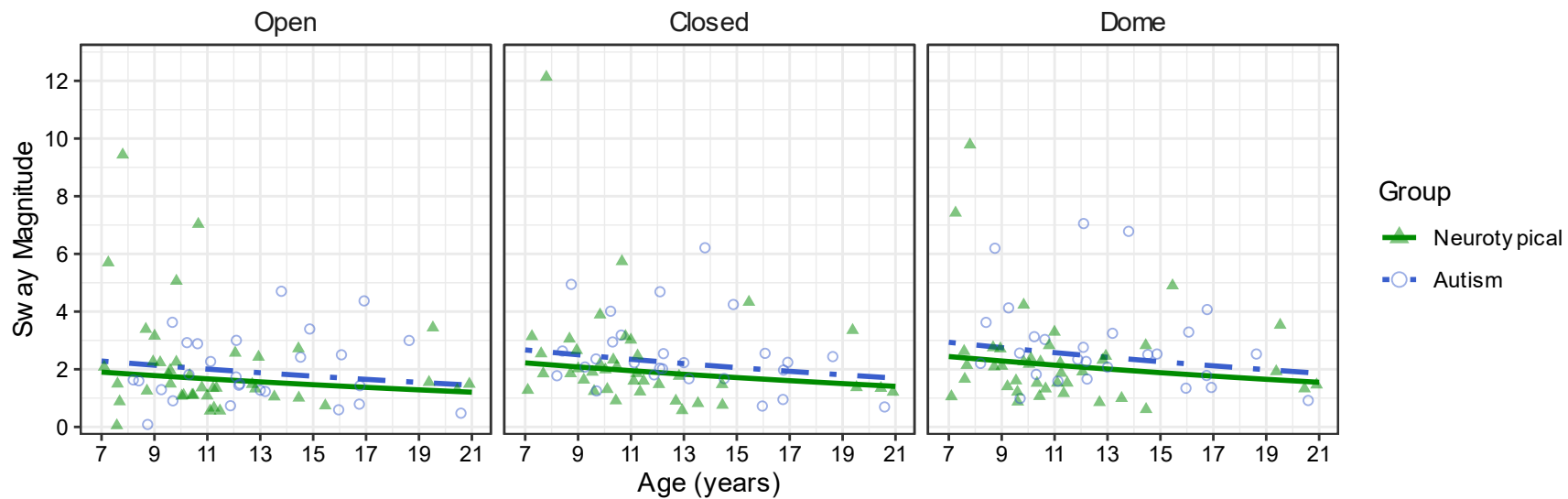


Figure 1. Sway magnitude differs by condition but follows a similar age trajectory in autism and neurotypical participants, with less stability in the Eyes Closed and Dome conditions compared to Eyes Open.

Sway variability

A generalized linear mixed-effects model with a Gamma distribution and a log link regressing sway variability onto group, age, and condition indicated differences within each of the factors but no interactions (Figure 2). There was a significant main effect of group ($\chi^2_1=5.26$, $p=.022$, Figure 2). Autistic participants ($M=1.25$, $SE=0.11$) showed greater sway variability compared to neurotypical participants ($M=0.96$, $SE=0.07$). There was a significant main effect of age ($\chi^2_1=14.85$, $p.001$, Figure 2), with sway variability decreasing as age increased ($\beta=-0.06$). There was a significant main effect of condition ($\chi^2_2=108.87$, $p.001$, Figure 2). Participants showed greater sway variability in the EC ($M=1.24$, $SE=0.08$, $p.001$) and Dome ($M=1.27$, $SE=0.08$, $p.001$) conditions compared to the EO condition ($M=0.836$, $SE=0.05$). Sway variability was not significantly different between the EC and Dome conditions ($p=.860$).

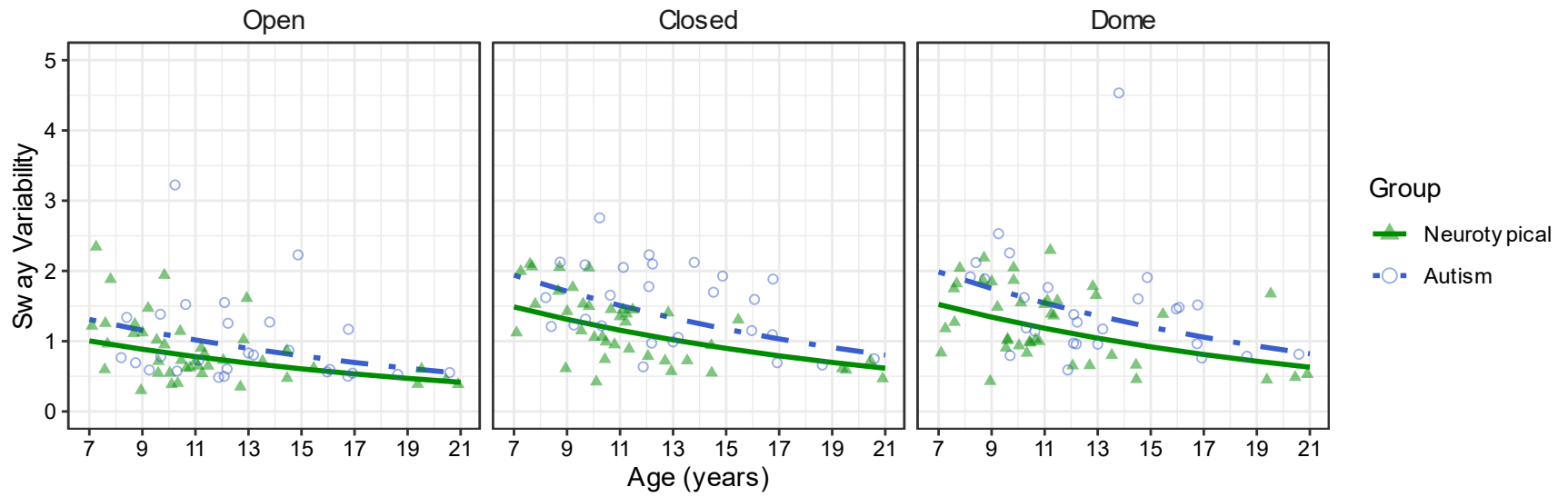


Figure 2. Sway variability differs by group but follows a similar age trajectory in autism and neurotypical participants, such that sway generally decreases with age and increases with condition difficulty.

DISCUSSION

Postural stability is critical for a wide range of activities of daily living, including those necessary for independence (Melzer et al., 2004). There is a gap in the current literature with respect to the age trajectory of postural stability in autism through childhood and adolescence, despite similar work in neurotypical children (Assaiante et al., 2005). We addressed this gap by assessing postural stability and sensory reweighting in autistic and neurotypical children and adolescents. Our findings demonstrate that autistic individuals have lower postural stability than neurotypical individuals throughout childhood and adolescence. Additionally, our findings indicate that these differences are consistent across visual conditions.

Postural stability decreases with changes or loss of visual information

Both autistic and neurotypical participants showed differing levels of postural stability across the CTSIB conditions. Participants' sway magnitude was greater in the EC and Dome conditions compared to the EO condition. This indicates that both groups had difficulty reweighting their reliance on vision to maintain postural stability based on the lack of visual information (EC condition) or the quality of the visual information they were receiving (Dome condition).

By examining sway variability within each of the conditions (EO, EC, Dome), we characterized differences in postural stability between autistic and neurotypical participants. As expected, autistic participants demonstrated lower postural stability than neurotypical participants. Contrary to our hypothesis and previous findings (Bucci et al., 2017; Dumas et al., 2016; Goh et al., 2018), however, the differences in postural stability that we observed between autistic and neurotypical participants were consistent across the three visual conditions. These findings indicate that autistic participants did not rely more heavily on vision to support postural stability than neurotypical participants, suggesting that sensory reweighting ability may not have been different between groups. There is a precedent for this, as some previous findings have shown that autistic participants do not rely more on vision for postural stability compared to neurotypical participants (Morris et al., 2015; Lim et al., 2018). This adds to the mixed literature on the role of visual information in postural stability for autistic individuals. Further research is needed to determine if the reweighting differences reported in other studies only manifest under more difficult task conditions (e.g., when standing on a compliant surface, reducing the availability of reliable proprioceptive input) or are only evident in a subset of autistic individuals.

Age differences in sway variability between autistic and neurotypical individuals

Autistic participants showed more sway variability across conditions from childhood into adolescence compared to neurotypical individuals. This indicates that autistic participants not only show differences in postural stability in childhood, but that these differences continue through adolescence. This is similar to previous findings that indicate that autistic individuals

have delayed postural stability development (Minshew et al., 2004) and that neurotypical individuals' postural stability continues to develop through adolescence and into adulthood (Goulème, et al., 2018; Shams et al, 2020).

These findings indicate that autistic and neurotypical individuals follow similar age trajectories of postural stability, but autistic individuals consistently demonstrate lower postural stability as measured by sway variability. Further, these findings suggest that postural stability continues to develop throughout the second decade of life, beyond the age range of many studies of the development of postural stability. This may be a specific consequence of motor development, a reflection of the influence of cognitive development (e.g., attention), or a combination of factors. More research is needed to further elucidate the mechanisms underlying the development of postural stability in adolescence and early adulthood.

STUDY 2

While static postural stability is an important building-block skill for development of other motor abilities, dynamic postural control is a stronger predictor of fall risk and functional mobility (Holbein-Jenny et al., 2007; Le Mouel & Brette, 2017; Robinovitch et al., 2013). Thus, it is necessary to assess both static and dynamic stability in order to fully understand the nature of postural control in autism. Here, we examined the spatial and temporal efficiency of movements during a dynamic postural control task. We used these measures to assess the development of dynamic postural control among autistic and neurotypical children and adolescents. Based on Miller et al. (2018), we predicted that autistic individuals would have consistently less efficient postural control than their neurotypical peers.

METHOD

Participants

We tested autistic ($n=21$, Male=19, Female=2; $M_{age}=12.73$ years, $SD_{age}=2.90$ years, $range=8.20-16.93$ years) and neurotypical ($n=32$, Male=13, Female=19; $M_{age}=10.60$ years, $SD_{age}=1.94$ years, $range=7.42-15.46$ years) children and adolescents. Participants reported their race as American Indian/Alaska Native (1.92%), Asian (1.92%), Black/African American (7.69%), or White (86.54%). Some participants declined to report their race (1.92%). Additionally, 26.92% of participants reported being of Hispanic ethnicity. The same diagnostic and exclusion criteria as Study 1 were used, as were the same IRB approval, consent, and assent processes.

Limits of Stability

The Limits of Stability task (LOS) is used to assess dynamic postural control by measuring how well a person can control their center of gravity outside of their base of support, without needing to move their feet or take a compensatory step to regain balance. Participants stood on the hard surface of a portable 20Hz force plate (BioSway, Biodex Corp.).

Targets and a user-controlled object were displayed at approximately eye-height on a screen in front of the participant. The participant used their center of gravity to move the user-controlled object to target locations by leaning their body without moving their feet (Figure 3). The LOS task includes nine target locations: eight at 75% of the typical limit of stability (6°: Forward, Forward Left, Forward Right, Left, Right; 4.5°: Backward Left, Backward Right; 3°: Backward), and one target at 0° (Center). Participants' foot position was recorded prior to data collection; any deviation from the original position was corrected prior to the start of the next target. Individual trials in which participants did not keep their feet firmly on the surface of the force plate (e.g., took a step, raised their heels, moved their feet) were discarded and, whenever possible, readministered after correcting foot placement.

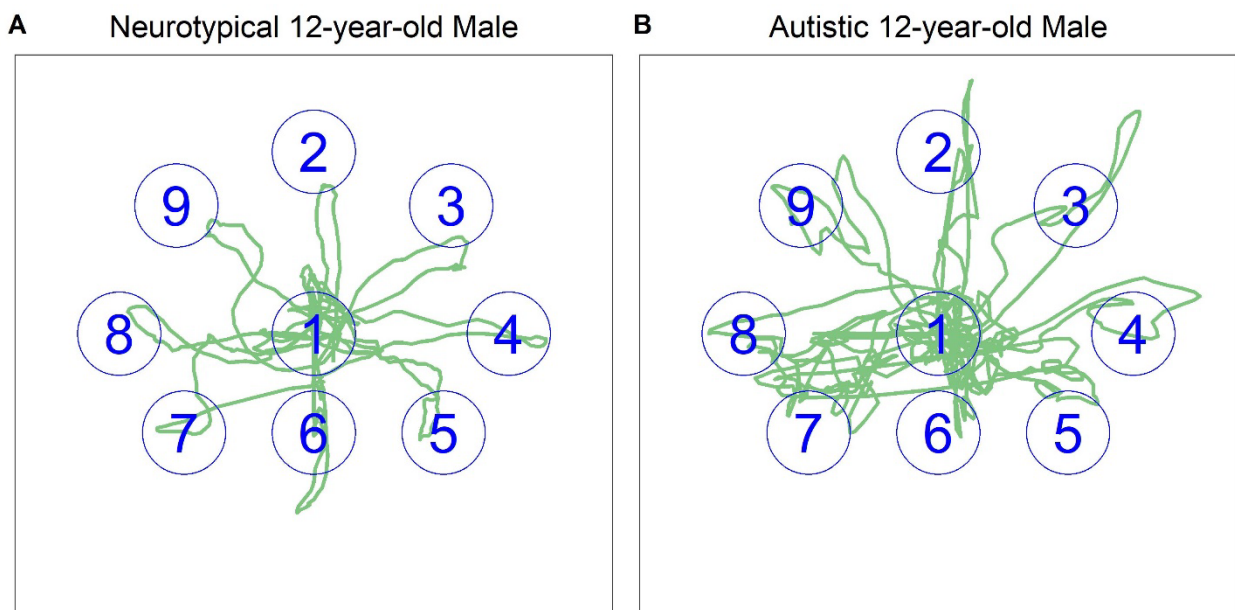


Figure 3. Sway plots of a (A) neurotypical or (B) autistic 12-year-old male participant during the Limits of Stability Task. 1=Center, 2=Forward, 3= Forward/Right, 4=Right, 5=Backward/Right, 6=Backward, 7=Backward/Left, 8=Left, 9=Forward/Left. Note: Target position is correct, but size is approximated for plotting purposes.

Data Analysis

The BioSway system records the total task completion time (*completion time*) and calculates an efficiency index (*movement efficiency*). Movement efficiency, as defined by the BioSway system, is the straight-line distance from the center of the force plate to the target divided by the actual distance traveled by the participant to the target (Supplementary Material

3). Higher movement efficiency scores indicate more direct movement to targets. Completion time and movement efficiency were analyzed with the same approach as Study 1.

RESULTS

Completion Time

A generalized linear model with a Gamma distribution and a log link was used to regress completion time onto group and age. There was a main effect of group ($\chi^2_1=13.90$, $p<.001$, Figure 4). Autistic participants ($M=57.21$, $SE=3.99$) used more time to complete the LOS task compared to neurotypical participants ($M=40.59$, $SE=2.19$). There was also a main effect of age ($\chi^2_1=12.77$, $\beta=-0.06$, $p<.001$, Figure 4), such that as participants' age increased, the time they used to complete the LOS task decreased.

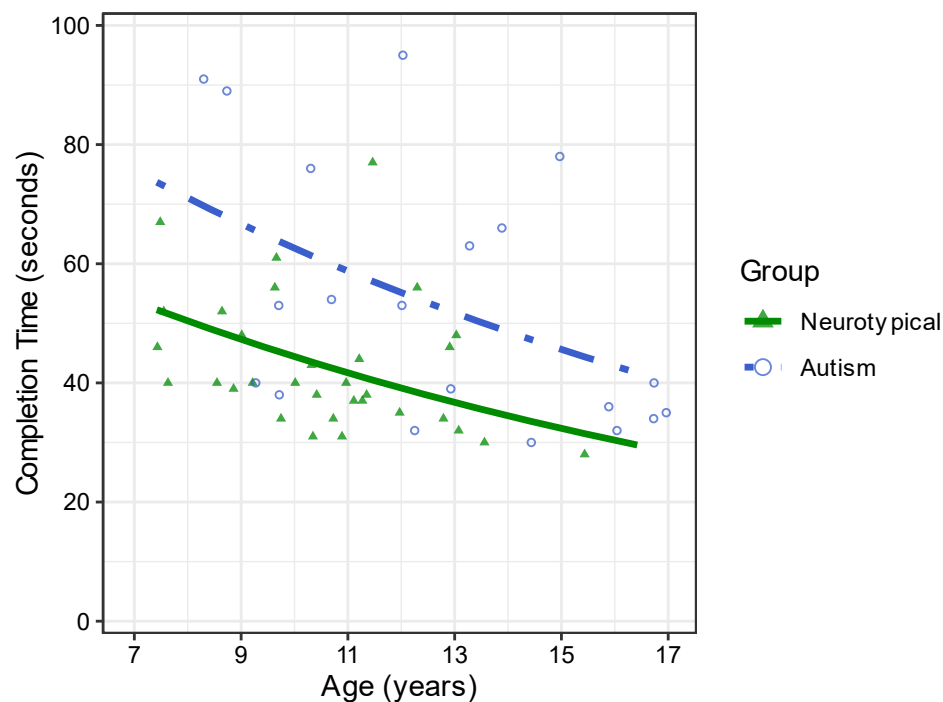


Figure 4. Autistic participants used more time to complete the LOS task compared to neurotypical participants, and both groups used less time as age increased.

Movement Efficiency

A linear mixed effects model was used to regress movement efficiency onto group, age, and target (center, forward, forward/right, right, backward/right, backward, backward/left, left, forward/left) with a random intercept by participant. There was a main effect of group ($\chi^2_1=20.08$, $p<.001$, Figure 5). Neurotypical participants ($M=51.88$, $SE=2.16$) were more efficient

when moving to targets than autistic participants ($M=35.84$, $SE=2.80$). There was a main effect of age ($\chi^2_1=34.55$, $\beta=4.05$, $p.001$), such that as participants' age increased their movements were more efficient. There was a main effect of target ($\chi^2_8=140.25$, $p.001$, Figure 5). See Table 1 for target pairwise comparisons.

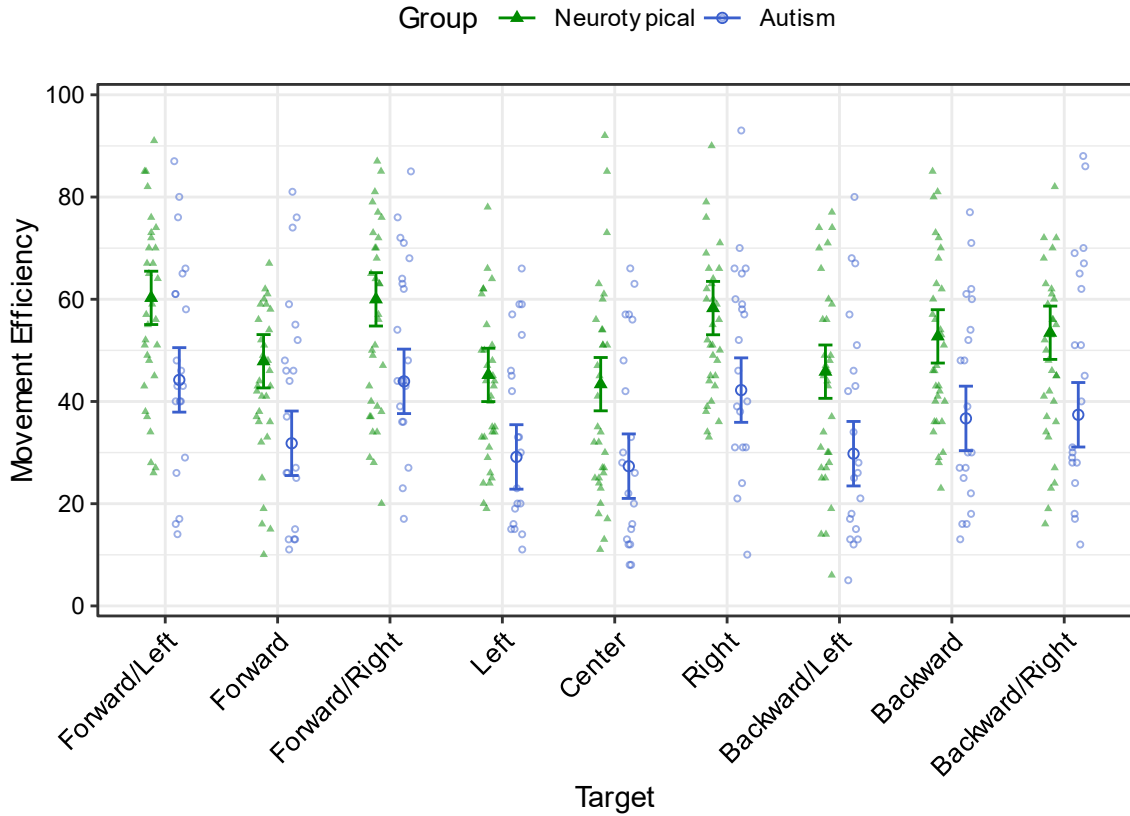


Figure 5. Autistic participants made less efficient movements to each of the targets compared to neurotypical participants. Error bars indicate 95% confidence limits.

Table 1

Pairwise comparisons of Movement Efficiency between targets

Target Contrast	Estimated Mean Difference	t ratio	p value
Forward/Left – Forward*	12.40	5.50	<.001
Forward/Left - Forward/Right	0.29	0.13	1.000
Forward/Left - Left*	15.08	6.69	<.001
Forward/Left - Center*	16.88	7.49	<.001
Forward/Left – Right	2.00	0.89	.994
Forward/Left - Backward/Left*	14.44	6.41	<.001
Forward/Left - Backward*	7.54	3.34	.025
Forward/Left - Backward/Right	6.83	3.03	.065
Forward - Forward/Right*	-12.12	-5.37	<.001
Forward – Left	2.67	1.19	.959
Forward – Center	4.48	1.99	.553
Forward - Right*	-10.40	-4.61	<.001
Forward - Backward/Left	2.04	0.90	.993
Forward - Backward	-4.87	-2.16	.435
Forward - Backward/Right	-5.58	-2.47	.248
Forward/Right - Left*	14.79	6.56	<.001
Forward/Right - Center*	16.60	7.36	<.001
Forward/Right – Right	1.71	0.76	.998
Forward/Right - Backward/Left*	14.15	6.28	<.001
Forward/Right - Backward*	7.25	3.22	.037
Forward/Right - Backward/Right	6.54	2.90	.092
Left – Center	1.81	0.80	.997
Left - Right*	-13.08	-5.80	<.001
Left - Backward/Left	-0.63	-0.28	1.000
Left - Backward*	-7.54	-3.34	.025
Left - Backward/Right*	-8.25	-3.66	.009
Center - Right*	-14.88	-6.60	<.001
Center - Backward/Left	-2.44	-1.08	.976
Center - Backward*	-9.35	-4.15	.001
Center - Backward/Right*	-10.06	-4.46	<.001
Right - Backward/Left*	12.44	5.52	<.001
Right – Backward	5.54	2.46	.257
Right - Backward/Right	4.83	2.14	.447
Backward/Left - Backward	-6.90	-3.06	.059

Backward/Left - Backward/Right*	-7.62	-3.38	.022
Backward - Backward/Right	-0.71	-0.32	1.000

Note. Standard error was 2.25 and degrees of freedom were 424.16 for all pairwise comparisons. * indicates p.05.

DISCUSSION

Many daily living activities rely heavily on dynamic postural control (Haddad et al., 2013). Despite this importance, there is little research examining dynamic postural control in autistic individuals relative to the body of work on static postural control (Lim et al., 2017). We addressed this gap by assessing dynamic postural control in autistic and neurotypical children and adolescents. We present data demonstrating that autistic individuals use less efficient dynamic postural control compared to neurotypical individuals across late childhood and adolescence.

Decreased movement efficiency during dynamic postural tasks

Autistic individuals used more time and longer paths to complete the limits of stability (LOS) task compared to neurotypical individuals. This is likely due to differences in overall dynamic postural control and the motor strategies autistic individuals use to compensate for these differences (Bojanek, et al 2020; Fournier et al., 2010; Miller et al., 2021). In previous work, Bojanek and colleagues demonstrated that autistic individuals constrain their postural sway by increasing the rigidity of their movements. This allows maintenance of balance, but limits movement efficiency during dynamic tasks (Bojanek et al., 2020). Difficulty with dynamic postural control in autism may be due to well-documented differences in underlying neural networks controlling movements. Decreased movement efficiency may indicate decreased neural connectivity between brain regions necessary for motor planning and modification of movements (Oldehinkel et al., 2020; Travers et al., 2015).

Age differences in dynamic postural control

Both autistic and neurotypical individuals used more efficient movements as age increased. Although autistic individuals used more efficient movements as age increased, their movements were continuously less efficient than that of neurotypical individuals. Thus, although autistic individuals follow expected age trajectories for motor control, they lag behind their neurotypical peers. Further research should investigate whether dynamic postural control is a malleable target for motor intervention in autism that could close the gap in motor development.

GENERAL DISCUSSION

Research on motor difficulties in autism has received renewed attention, with existing literature suggesting the presence of differences between autistic and neurotypical

development in motor abilities (Fuentes, Mostofsky, & Bastian, 2009; Mosconi et al., 2015) and their underlying neural mechanisms (Oldehinkel et al., 2020; Unruh et al., 2019; Wang et al., 2019). Although these studies demonstrate that motor difficulties in autism persist across childhood, adolescence, and adulthood (Bhat et al., 2011), there remains a dearth of literature on the long-term functional impact of motor problems or on their age trajectories. Here, we present two studies with community-derived samples demonstrating that autistic individuals (1) have lower static postural stability and (2) use less efficient dynamic postural control compared to neurotypical individuals across childhood and adolescence.

Previous work in other clinical populations demonstrates a relationship between low postural stability, limitations in activities of daily living, and reduced quality of life (e.g., cerebral palsy; Pavão, Dos Santos, de Oliveira, & Rocha, 2014; stroke, Hsieh, Sheu, Hsueh, & Wang, 2002), and low postural stability is predictive of fall risk in older adulthood (Melzer et al., 2004; Swanenburg, de Bruin, Uebelhart, & Mulder, 2010). There is little published literature on the specific relationship between postural control and activities of daily living in autism, but emerging work suggests that low postural stability is associated with poorer performance on activities of daily living, particularly for individuals with lower-than-average IQ (Fisher et al., 2018). Given the results presented here, it is concerning that only an estimated 19.5% of autistic individuals receive physical therapy, and only 48.5% receive occupational therapy (largely in the context of academic skills like handwriting or self-care skills like dressing) (Zablotsky et al., 2015). Many of those who do receive physical therapy typically discontinue services after early motor milestones are met (e.g., crawling, standing, walking) and physical therapy service utilization drops sharply as age increases (Cidav et al., 2013), despite the fact that motor problems persist. This lack of support for motor development in autism may have a detrimental effect on quality of life. Research is needed to determine if there is a relationship between postural stability, daily living skills, and quality of life in autism.

We used a community-based assessment approach to reduce barriers to participation (George, Duran, & Norris, 2014; Luebbert & Perez, 2015). This approach substantially increased the racial and ethnic diversity of the current samples compared to previous autism studies, with nearly twice as many Black participants and ten times as many Hispanic participants reported in other samples (West et al., 2016). This community-based approach can be used to expand the breadth of those included in autism research, improving access for participants from under-represented racial and ethnic backgrounds, lower socioeconomic backgrounds, or with limited transportation or childcare. By using short, easily-understood study protocols that limit the cognitive demands and level of language required to participate, we can also include participants with a wider range of intellectual abilities and co-occurring conditions. Thus, study samples will be more reflective of the broader autism population, including those whose resources and abilities may have prevented them from participating in traditional lab- or clinic-based research. This will further improve the generalizability of autism research and improve evidence-based clinical care.

Static postural stability and dynamic postural control are a clinically-relevant issues that may hinder an individual's ability to efficiently and effectively complete activities of daily living (for review, see Haddad et al., 2013). It is important to characterize the age trajectory of postural stability and control in autistic children and adolescents, both to inform interventions that target these building-block skills, and to support public policies and clinical practice guidelines that facilitate access to motor intervention across the lifespan.

CONTRIBUTIONS

Contributed to conception and design: HLM, NLB, RMP

Contributed to acquisition of data: HLM, GMS

Contributed to analysis and interpretation of data: NEF, HLM, TNT

Drafted and/or revised the article: NEF, HLM

Approved the submitted version for publication: NEF, GMS, TNT, NLB, RMP, HLM

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Out of respect for preferences expressed by many autistic self-advocates in our studies and in the community, we have chosen to use identity-first (rather than person-first) language throughout this manuscript. In doing so, it is not our intention to diminish or invalidate the preferences or perspectives of those who prefer person-first language. We continue to welcome feedback on ways that we can effectively partner with the autistic community to advocate for respect, acceptance, inclusion, and representation in research.

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SUPPLEMENTARY MATERIAL 1.

The following equation is used to calculate sway magnitude:

$$\text{Sway magnitude} = \frac{\sum_{i=1}^n \sqrt{X_i^2 + Y_i^2}}{n} / 100$$

where X and Y are the participant's sway angles in the X and Y direction for a given sample (*i*) in a trial with *n* samples.

SUPPLEMENTARY MATERIAL 2.

The following equation is used to calculate sway variability:

$$\text{Sway variability} = \sqrt{\frac{\sum_{i=1}^n (X_i - \bar{X})^2 + (Y_i - \bar{Y})^2}{n}} / 100$$

where X and Y are the participant's sway angles for a given sample (i) and \bar{X} and \bar{Y} are the participant's mean sway angles in their respective directions for n samples in a trial.

SUPPLEMENTARY MATERIAL 3.

The following equation is used to calculate movement efficiency:

$$\text{Movement Efficiency} = \left(\sqrt{(a - q)^2} / \sqrt{\sum_{i=1}^n (p_i - p_{i-1})^2} \right) * 100$$

where a is the center of the force plate, q is the target location on the force plate, p is the participant's center of force location on the force plate for given sample (i) in a trial with n samples.

DATA ACCESSIBILITY

The data and code for this paper are currently in the process of being transferred from one university to another. As there are ongoing discussions about the rights and obligations for this data and code, it cannot be shared at this time.

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